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Comparison of noninvasive imagery methods to observe healthy and degenerated olfactory epithelium in mice for the early diagnosis of neurodegenerative diseases

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2 ABSTRACT

Olfactory dysfunction could be an early and reliable indicator for the diagnosis of 3 4 neurodegenerative disorders such as Alzheimer and Parkinson's diseases. In this paper, we compare the potential of different noninvasive medical imaging modalities (optical coherence 5 6 tomography, confocal microscopy, and fluorescence endomicroscopy) to distinguish how the olfactory epithelium, both at the cellular and the structural levels, is altered. Investigations 7 were carried out on three experimental groups: two pathological groups (mice models with 8 9 deliberately altered olfactory epithelium and Alzheimer's disease transgenic mice models) were compared with healthy mice models. As histological staining, the three tested noninvasive imaging 10 tools demonstrated the general tubular organization of the olfactory epithelium on healthy mice. 11 12 Contrary to OCT, confocal microscopy and endomicroscopy allowed visualizing the inner structure 13 of olfactory epithelium as well as its morphological or functional changes on pathological models, alterations classically observed with histological assessment. The results could lead to relevant 14 development of imaging tools for noninvasive and early diagnosis of neurodegenerative diseases 15 through the in situ characterization of the olfactory epithelium. 16

17 Keywords: epithelium olfactory, medical imaging, optical biopsy, neurodegenerative diseases, Alzheimer disease.

1 INTRODUCTION

Recent studies have shown a strong correlation between impaired olfactory perception of patients and 18 neurodegenerative conditions, such as Alzheimer's disease (AD) (Kjelvik et al., 2014; Wesson et al., 2010; 19 Wang et al., 2010; Arnold et al., 1998), Parkinson's disease (Doty, 2012; Berg, 2008), frontotemporal 20 dementia (Alves et al., 2014; McLaughlin and Westervelt, 2008) and Huntington's disease (Lazic et al., 21 2007; Barresi et al., 2012). These works lead to consider olfactory dysfunction as an early marker of 22 neurodegenerative conditions and as a relevant indicator for early-stage diagnosis of such diseases. For 23 instance, in AD, odor detection, discrimination and identification are affected earlier than cognitive 24 performances as demonstrated in several studies on patients (Wang et al., 2010; Arnold et al., 1998; Talamo 25 et al., 1991), as well as on different animal models, in particular mice (Sohrabi et al., 2012; Wu et al., 2013; 26 Alvarado-Martínez et al., 2013). These functional olfactory alterations are probably due to early Amyloid- β 27 peptide deposits in the olfactory epithelium (OE) leading to cellular apoptosis and a decrease of dendritic 28 spine densities (Yao et al., 2017). These studies have identified a need to investigate, in a more advanced 29 manner, the area of the nasal cavity which concentrates part of the olfactory functionalities in order to 30 establish reliable biomarkers of AD. This will serve to both improve diagnosis and to surrogate markers of 31 efficacy during clinical trials (Quinn, 2013). Olfactory epithelium is a pseudo-stratified neuroepithelium 32 covering 10% of the nasal cavity and responsible of odor detection. It is characterized by three main 33 cell types that can be clearly identified: the olfactory sensory neurons constituting the receptor cells for 34 trapping odor molecules, the supporting cells and the basal stem cells that continuously regenerate olfactory 35 neurons (Holbrook et al., 1995; Barrios et al., 2014). Reaching the OE for in vivo characterization and 36 monitoring of the neural organization (Fig. 1) is still an open scientific and clinical challenge because of its 37 38 location and access pathway as demonstrated in our recent work (Girerd et al., 2018). To the best of our knowledge, no conventional instrument can be used to non-invasively reach this area. To overcome this 39 problem, we are developing a microrobotic solution based on a concentric tube robot mechanism (flexible 40 robotic endonasal system), which embeds the optical characterization tool such as miniature Optical 41 Coherence Tomography (OCT), confocal or endomicroscopy probe. This work is investigated within the 42 translational and multi-disciplinary NEMRO project¹ that aims at identifying neuropathological changes 43 and early signs of degeneration within the human olfactory tissue for earlier diagnosis of neurodegenerative 44 diseases. More precisely, the work carried out consisted in developing a nasal endoscopic system based on 45 the use of flexible continuum robot of less than 2mm of diameter able to navigate without collision within 46 the nasal slots. The endoscopic system can be equipped, thanks to its inner free channel, with a fiber-based 47 imaging probe (i.e., OCT, confocal, or endomicroscopy) for in situ characterization of the OE. Pending 48 the design of this new system, we have implemented a series of experiments to the ability of the imaging 49 tools to: (i) distinguish the structural shape of the OE on healthy mice by comparing the results with those 50 using conventional histological assessment, and (ii) identify morphological alterations and early signs of 51 52 degeneration using pathological mice models (ZnSO4 lesion, APPswe/PSEN1E9 mice model of AD).

53 Confocal microscopy, OCT and endomicroscopy are widely studied in both research investigations 54 and clinical purposes, especially in ophthalmology and dermatology. The images produced by these 55 imaging systems are also known as optical biopsies able to visualize biological tissues both in depth and 56 at micrometer resolution while being non-invasive. For instance, OCT has demonstrated the ability to 57 investigate cytoarchitecture in the brain (Ibne Mokbul, 2017) and to observe, among others, human nasal 58 epithelium (Mahmood et al., 2006; Oltmanns et al., 2016). Confocal microscopy, a less recent technology 59 compared to the other two, has become an interesting investigation technique in medicine (Fine et al.,

¹ Microrobotic nasal endoscopy by OCT: impact of smell deficiency on neurodegenerative diseases.



Figure 1. Representation of nasal anatomy, structure, and the OE shape and location (Girerd et al., 2018).

1988; Hofmann-Wellenhof et al., 2012). Concerning the endomicroscopy such as the CellVizio technology,
it is more recent and has proven real benefit for in vivo diagnosis of some diseases, namely for GI tract
applications (De Palma, 2009; Mielke et al., 2015).

The experimental scenario carried out in this paper consisted in studying the potential of each of the 63 selected imaging modalities to observe alterations (at the structural or cellular levels) that are involved 64 within the OE tissues. To do this, two groups of mice were used: (i) mice received a bilateral $ZnSO_4$ 65 66 irrigation of the nasal cavity to induce morphological alterations of the OE (Ducray et al., 2002; McBride et al., 2003; Bon et al., 2005), and (ii) double transgenic APPswe/PSEN1E9 mice (Jackson Laboratory, 67 68 USA)². They are mouse model of AD whose mutations targeting Amyloid precursor protein and presenilin 1 69 genes (APP/PS1) are associated with early-onset of Amyloid- β peptide within the OE and the brain resulting in learning and memory deficits (Wu et al., 2013; Yao et al., 2016). 70

71 The preliminary conclusions from these experiments show that OCT allowed visualization of the general 72 structural aspect i.e., turbinates of the OE tissues, as well as the overall disorganization of the olfactory tissue 73 induced by ZnSO4 irrigation. However, due to the limited spatial resolution of the OCT system, this imagery tool does not allow observation at a cellular level, contrary to confocal microscopy and endomicroscopy, 74 75 the pseudo-stratified structure of the OE. Indeed, confocal microscopy and endomicroscopy allowed 76 visualizing, similarly to the histological assessment, the inner and pseudo-stratified structure of OE, i.e., 77 cell bodies, axons and the different cell layers of the epithelium. Otherwise, morphological changes (i.e., disorganization and reduction of the thickness of the different layers that form the OE) after ZnSO4 78 treatment that are traditionally observed with histological procedure were well observed by the three 79 imaging systems. Concerning the visualization of possible Amyloid- β peptides occurring within the 80 tissues sampled from APPswe/PSEN1E9 mice, only the endomicroscopy device (fluorescence confocal 81 microscopy) pointed out possible connected fluorescent dots within the OE. 82

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2 MATERIALS AND METHODS

83 2.1 Animal Models

Swiss female mice (Janvier Labs, FR)³ and APPswe/PSEN1E9 mice aged 3-4 months were maintained under both standard and controlled laboratory conditions (12h:12h under light/dark cycle) with food and water available ad libitum. All animal experiments comply with the ARRIVE (Animal Research: Reporting of In Vivo Experiments⁴) guidelines and are carried out in accordance with the European Directive 2010/63/EU⁵ for the care and the use of living animals for laboratory experiments.

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90 **2.2** $ZnSO_4$ Lesion

To identify the ability of the studied optical imaging tools to visualize large deterioration incurred within 91 the OE tissues, mice received a bilateral intranasal application of $ZnSO_4$ solution (Sigma Aldrich, FR)⁶ 92 under general anaesthesia (isoflurane). Intranasal infusion of $ZnSO_4$ is one of the most commonly used 93 methods to induce a massive destruction of mature olfactory neurons and decrease odor sensitivity a few 94 days after $ZnSO_4$ perfusion (Ducray et al., 2002). Mice were placed on their back, and each nostril was 95 injected with 8μ l of a sterile 10% ZnSO₄ solution in 0.9% sodium chloride. Immediately after ZnSO₄ 96 irrigation, mice were held with their head down for several seconds to minimize spread of the solution to the 97 oral cavity. Since regeneration of the OE typically occurs within 7 days after $ZnSO_4$ application, mice were 98 perfused 4 days after the intranasal application to keep them in condition of massive alterations (McBride 99 et al., 2003). 100

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102 2.3 Tissues Preparation

Mice were transcardially perfused with 4% paraformaldehyde in phosphate-buffered saline (PFA in PBS) to fix tissues. The OE tissues were then removed, post-fixed overnight in 4% paraformaldehyde and cryoprotected with a 15% sucrose solution for 24h. The tissue samples were either embedded in Tissue Tek for histological experiments or kept in PBS for a few hours before observation with the OCT and the confocal microscopy imaging tools.

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109 2.4 Histology and Immunohistochemistry

Frozen coronal and sagittal sections of 10μ m were obtained using a cryostat, mounted onto clean, subbed slides, and stored at -20° C until processing. Three different protocols were carried out as described above:

- To visualize the internal structure of OE, tissue sections were rehydrated and stained with haematoxylineosin during two minutes. Sections were then dehydrated, and cover-slipped with Canada balsam (Carl
- 114 Roth).

• Immunohistochemistry was performed in three APPswe/PSEN1E9 mice in order to visualize Amyloid- β aggregates within their OE. After rinsing in PBS-Triton (PBS-T) 0.3%, sections were exposed to polyclonal rabbit anti-Amyloid- β primary antibody (1:100; ab2539, Abcam) in milk solution (PBS-T,

- 118 1% BSA, 10% lactoprotein) for 24h at 4°C. After several washings, sections were exposed 2h at room
- temperature to either the fluorescent goat anti-rabbit IgG (1:1000, Alexa Fluor 488, Invitrogen) or the
- 120 biotinylated secondary horse anti-rabbit IgG (1:500, Vector Laboratories) in PBS. After the incubation

³ www.janvier-labs.com/en

⁴ www.nc3rs.org.uk/arrive-guidelines

⁵ eur-lex.europa.eu/legal-content/EN/TXT/?uri=celex%3A32010L0063

⁶ www.sigmaaldrich.com

in biotinylated secondary antibody, OE slices were exposed to an avidin horseradish peroxidase
complex (ABC Elite kit, Vector Laboratories) for 1h at room temperature. The peroxidase complex was
visualized after a 10-minute exposure to a chromogen solution containing 0.04% 3.3' diaminobenzidine
tetrahydrochloride (DAB, Sigma Aldrich) with 0.006% hydrogen peroxide in PBS. Sections were then
rinsed in PBS, stained with toluidine blue for 30 seconds and finally dehydrated and cover-slipped
with Canada balsam (Roth).

• Images were produced from an Olympus microscope $B \times 51$ set up witha $\times 20$, $\times 40$ or $\times 60$ objectives 127 equipped with an Olympus DP50 camera (Axio Imager Zeiss). To observe Amyloid- β aggregates 128 within the entire OE using a CellVizio imaging device (Mauna Kea Technologies⁷ Paris, FR), we 129 adapted the immunohistochemistry protocol, normally performed on brain slices, on the whole OE 130 tissue. OE of two APPswe/PSEN1E9 mice were treated with a PBS-T 0.3% solution during 20 minutes 131 to make the tissue sample permeable. Then, samples were exposed for 44h at 4°C to polyclonal rabbit 132 anti-Amyloid- β primary antibody (1:100, ab2539, Abcam) in milk solution (PBS-T, 1% BSA, 10% 133 lactoprotein). After several washings, sections were exposed (4h at room temperature) to the secondary 134 goat anti-rabbit IgG (1:1000, Alexa Fluor 488, Invitrogen). Olfactory epithelium tissues were then 135 rinsed in PBS and observed with the CellVizio device. 136

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138 2.5 Medical Imaging Devices

The imaging modalities that were selected for the characterization of OE tissues are widely used in clinical
applications (Fig. 2). The images are commonly referred to as optical biopsies because of their ability to
visualize biological tissues in depth and at micrometre resolution almost similar to a histopathological
study. In addition, these images are available in a miniaturized version (or can be miniaturized) to be used
in vivo by passing through natural orifices such as the nasal slots or through small artificial orifices.



Figure 2. Photography of the studied imaging tools: (a) OCT, (b) confocal microscopy, and (c) CellVizio endomicroscopy probe.

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144 2.5.1 Optical Coherence Tomography

OCT allows observing the different tissue layers (by penetrating into the scattering medium) in aim to
 capture micrometer-resolution images (i.e., optical biopsies) and in nondestructive way. The Vivosight

www.maunakeatech.com/en/cellvizio

OCT device (Fig. 2A) (Michelson Diagnostics⁸, UK), initially developed for clinical dermatology, was 147 tested in this work. It uses a multi-beam swept-source frequency domain OCT (SS-OCT) equipped with 148 a $\lambda = 1300$ nm wavelength light source, which offers an accurate in vivo and in-depth characterization 149 (up to 2mm) of biological tissues thanks to an optical resolution of 7.5 μ m and 5 μ m laterally and axially, 150 respectively. Three optical biopsy modes are provided by with the OCT system: optical core (1D z-signal), 151 cross-sectional slices (2D images), and volumes. This kind of imaging tool was used in few studies on 152 animal models which demonstrated that OCT is effective in the visualisation of rat olfactory bulb (Watanabe 153 et al., 2011) and mice hippocampus (Chong et al., 2015) or olfactory epithelium (Ueda et al., 2019). 154

The Vivosight OCT device was used in our work in order to visualize the different OE layers sampled from both the healthy and pathological mice. The OCT data were used to compare structurally the OE structure, shape, and thickness for both groups. The results are discussed and compared to the other imaging tools as well as the histological results reported in Section 3.

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160 2.5.2 Confocal Microscopy

VivaScope 1500 (Fig. 2B)(Mavig GmbH⁹, DE) is typically used to observe and evaluate biological 161 tissues in both in vivo and ex vivo manners. Its current commercialized in vivo use in dermatology, allows 162 visualization through the epidermis and dermis until the reticular layer by just putting the probe onto 163 the skin of the patient with oil/gel interface, without any damage/pain. A laser beam (830nm) is used 164 and directed onto the skin area of interest and is then reflected forming (after a reconstruction phase) 165 grayscale and real-time micrometric resolution images of the tissue. The reflectance confocal microscopy 166 VivaScope 1500 is able to perform investigation on the tissue in the transverse plane of 5μ m of thickness 167 with a field-of-view of 500μ m × 500μ m. In addition, a software is provided, which allows tuning the laser 168 source power and then varying (with a step of 1.5μ m) the acquisition depth from the tissue surface up to 169 200μ m. The data can be arranged in a succession of 2D stacks. Additionally, a high-resolution actuator 170 equips the device. It allows moving laterally the confocal probe in x and/or y axes in order to enlarge the 171 172 initial field-of-view up to 8mm×8mm (almost the entire size of the mice OE). In the literature, this imaging tool was already evaluated in few studies for in vivo investigations and characterization of mice corneal 173 tissue (Lee et al., 2015; Chen et al., 2008). 174

The VivaScope device was slightly adapted to our study, by adding a designed sample holder, providing ergonomic adaptation for an ex vivo use. It allows to stabilize the sampled OE to avoid image artefacts induced by the probe motion during the scanning process. The optical biopsies are analyzed and compared in Section 3.

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180 2.5.3 CellVizio Endomicroscopy

181 The CellVizio endomicroscopy probe (pCLE) (Fig. 2C) is a standalone imaging system based on a fiber technology achieving real-time (9 to 12 images/second), high resolution, and in vivo optical subsurface 182 tissue characterization. It allows to make more targeted biopsies and to reach more areas that were previously 183 inaccessible for visualization. It has been demonstrated that pCLE can be used across a number of different 184 indications: biliary strictures, lung nodules, pancreatic cysts, urology and many other disciplines. The 185 CellVizio incorporates a proximally-scanned fiber bundle to deliver a 488nm wavelength laser light toward 186 to the sample and acquire a fluorescence signal, in return. In our study, we used the Z1800 probe which 187 incorporates a fiber bundle composed of 30,000 optical fibers, providing a lateral resolution of $3.5\mu m$ 188

⁸ www.vivosight.com

⁹ www.vivascope.de

189 with a field-of-view 512×448 pixels equivalent to 500μ m of diameter (the resulting image has the form 190 of a disk). Furthermore, the CellVizio system provides different types of flexible probes sized from 1mm 191 to 5mm (diameter) offering spatial resolutions of 1μ m to 3.5μ m, respectively able to observe tissues at 192 different depths ranging from 0μ m to 70μ m depending on the probe.

Furthermore, to visualize and characterize the sampled OE at the cellular level, we prepared a biochemical solution in which the sampled OE were previously soaked. To do this, we used the Acriflavine (Sigma-Aldrich), a fluorescent agent for labelling acidic constituents, to stain nuclei (by labelling RNA molecules) of the different structures of the OE (olfactory neurons layer, connective tissue, etc.). The main particularity of the pCLE device is the possibility to emphasize the presence of Amyloid- β peptides within OE tissues. To the best of our knowledge, no such work has been reported in the literature.

3 **RESULTS**

199 **3.1 Healthy Olfactory Epithelium**

As expected, in healthy mice, the main OE appeared as a pseudo-stratified structure organized in turbinates (Barrios et al., 2014) using histological assessment (Fig. 3A). In Fig. 3C, from the surface to the depth, we can see olfactory cilia (1-receptors), a thick layer of olfactory neurons and supporting cells $(\approx 160\mu m)$ (2), basal stem cells (3), the presence of blood vessels (4) and bundles of axons (5) within connective tissue.

The Vivosight OCT device was used for the real-time visualization of perfused OE. When, the turbinate structure of the OE could be clearly distinguished because of the different shades of gray visible in Fig. 3B, the spatial resolution ($\approx 5\mu$ m) did not allow to highlight its internal structural organization (i.e., olfactory neuronal layers) as shown in Fig. 3A and Fig. 3B (rectangular boxes).

The confocal microscopy device, which provided a higher resolution compared to OCT, allowed to 209 visualize both the general shape of the turbinates and the inner structure of the OE tissues, and to measure 210 its thicknesses ($\approx 140 \ \mu m$). Confocal images allowed to identify internal structures at almost cellular 211 scale, as demonstrated in (Fig. 3D and Fig. 3E). Indeed, the thin hyper reflecting and irregular superficial 212 layer corresponding to cilia receptors can be seen, as well as the layers of the olfactory neurons and the 213 axons bundles. Images produced during optical microscopic characterization (Fig. 3F) and the confocal 214 215 microscopy examination (Fig. 3G) were substantially identical and highlight the relevant use of confocal microscopy to explore and characterize OE tissue samples. Whereas the biochemical histology examination 216 requires sampling, sample preparation, labelling to assess the tissue features, using confocal microscopy 217 seems to be relevant for in vivo and non-invasive characterization. 218

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220 3.2 $ZnSO_4$ -induced Lesion of the Olfactory Epithelium

221 In order to evaluate and to compare the ability of the different optical tools to visualize major alterations within the OE, mice received an intranasal injection of $ZnSO_4$ solution under general anaesthesia 222 (isoflurane). Intranasal administration of $ZnSO_4$ is one of the most commonly used methods to induce 223 224 a massive destruction of mature olfactory neurons and decrease odor sensitivity a few days after the 225 treatment (Ducray et al., 2002). As demonstrated in Fig. 4C and E, an intranasal injection of $ZnSO_4$ solution strongly injured the OE, which appeared friable and disorganized, with a huge decrease in neuronal 226 227 layer thickness of the OE ($\approx 25 \mu$ m; as shown in Fig. 4C and Fig. 4E) compared to the OE sampled from 228 healthy mice (Fig. 3A). Moreover, disorganized cell bodies seemed degraded and blood vessels and bundles 229 of axons were no longer observed (Fig. 4E).



Figure 3. Olfactory epithelium tissues were observed using histology (remove-frozen-cut-HE stained) as shown in images A, C, and F. OE were also viewed using the OCT device as on image B. It highlights that the same region can be identified in both histology and OCT (e.g., the area marked with a white rectangle) which showed the general organization and structure of the OE. The VivaScope confocal microscopy system (D, E, G), as well as histology (C, F), allowed the observation at a cellular and layered level of the OE tissues such as cilia (1), neuronal layers (2), basement membrane (3), blood vessels (4), bundles of axons (5).

In the same manner, OCT technique allows visualizing a structural disorganization as well as a significant reduction of the thickness of OE after an intranasal administration of the $ZnSO_4$ solution (Fig. 4D). However, it remains challenging to accurately distinguish smaller variations or damages using the OCT tool due to its limited resolution. On the contrary, confocal microscopy is more suitable to visualize morphological changes of the OE at the cellular scale: bilateral $ZnSO_4$ irrigation of the nasal cavity damaged both at the cellular level (neuronal layers) and the general structure of the tissues (OE thickness $\approx 25 \mu$ m, see Fig. 4F) compared to healthy OE (Fig. 3A-B).



Figure 4. Illustration of the structural changes in OE tissue induced by bilateral $ZnSO_4$ irrigation of the nasal cavity. (A) and (B) show the histology and the OCT observations on healthy mice, respectively, when (C) and (D) show the tissue (at the turbinates level) after the bilateral $ZnSO_4$ administration which resulted, for instance, in a decrease in tissue thickness. Confocal examination (F) offers a cellular-level observation almost similar to the histological labelling (E) and confirms the decreased thickness of the neuronal layer (2, white bar) and the general disorganization of the connective tissue (6, absence of blood vessels and bundles of axons) after $ZnSO_4$ irrigation.

237 3.3 Mouse Model of Alzheimer Disease (APP/PS1 Mice)

As already established in (Wu et al., 2013), immunohistochemistry allows identifying Amyloid- β peptides within the OE neuronal layer of four months old APP/PS1 mice model of AD (Fig. 5B). As expected, OCT enables to visualize the turbinate structure and confocal microscopy enables to see the cellular organization

- 241 (layer of olfactory neurons and bundles of axons), the shape , and to measure the thickness (\approx 180 μ m) of
- 242 the OE of APP/PS1 mice (Fig. 5). However, none of these two tools give any visual clues concerning the presence of Amyloid- β peptide within the neurons layers or a decreased thickness of the OE of these mice.



Figure 5. OE tissues of young APP/PS1 mice (aged 4 months) was observed using OCT (A), immunohistochemistry (B) or confocal microscopy (C). Amyloid- β peptides were identified (black arrow) using immunohistochemistry with specific antibodies. However, OCT and confocal images failed to reveal these peptides or any alteration of the OE (2 (white bar) = neuronal layer; 4 = blood vessels; 5 (white stars) = bundles of axons).

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The 2mm diameter standalone endomicroscopy device was used in order to evaluate the possibility to 244 consider such system for in vivo investigation. The objectives are to visualize both the structural and the 245 functional alterations of OE (i.e., potential decrease of thickness and Amyloid- β peptides). Note that 246 CellVizio system requires the use of a fluorescence technique, which could potentially make its use on 247 patients less trivial in comparison to OCT or confocal microscopy. However, CellVizio system has already 248 been used in several clinical application with a well-established tissue labelling routine. Concerning our 249 study on animal OE tissues, as depicted in Fig. 6A, an immunohistochemistry followed by DAB revelation 250 performed in OE slices of old APP/PS1 mice (18 months) highlighted that Amyloid- β peptides were 251

organized in diffuse plaques with an irregular shape that appeared as a loose network and without a densecore when compared with 4-months-old mice.

254 the fluorescent labelling of Amyloid- β peptides of the OE slices using Additionally, immunohistochemistry (Fig. 6B) or of whole tissue using CellVizio endomicroscopy (Fig. 6C) allowed 255 visualizing the structural organization of the tissues. By analyzing Fig. 6B and Fig. 6C, it is possible to 256 257 clearly observe the OE inner structure (i.e. olfactory neurons layer (2) laying on connective tissue (1) with altered blood vessels (4)) and allowed thickness measurement of the tissue samples ($\approx 100 \ \mu m \ vs \approx 140$ 258 μ m for histological examination). Note that observations were more challenging due to the fact that the OE 259 seems "crumbly", possibly because of the older mice which lead to increase the number of Amyloid- β 260 deposits and senile plaques as demonstrated in (Wu et al., 2013; Yao et al., 2017). Presumed amyloid- β 261 peptides could be detected if we considered the very high brightness (compared to the rest of the tissues) 262 spots (white arrows in Fig. 6C), possibly due to the presence of anti-Amyloide- β primary antibody revealed 263 264 with fluorescent secondary antibody.



Figure 6. OE tissues sampled from old APP/PS1 mice (aged 18 months) was observed using classic (A) and fluorescent (B) immunohistochemistry or noninvasive CellVizio technology (C). (1 = connective tissue; 2 (white bar) = neuronal layer; 4 = presumed blood vessels; arrow = presumed Amyloid- β peptide).

4 DISCUSSIONS AND CONCLUSION

The comparison between conventional histology and noninvasive imaging techniques, such as OCT and 265 266 confocal microscopy, showed that OCT technique allowed for the macroscopic visualization of the nasal 267 cavity content. For instance, the turbinates as well as the overall OE can be distinguished using an OCT device, while observing the different cell layers within the OE is still more challenging. In addition, OCT 268 269 technique has demonstrated the possibility to observe major impairments of OE (e.g., epithelium thickness) after $ZnSO_4$ administration, although no specific results were obtained on aged APP/PS1 mice. On the 270 contrary, confocal microscopy allowed the observation of the macroscopic and microscopic organization of 271 272 the OE. In fact, it is possible to distinguish cell bodies, axons and the different cell layers within the OE tissues. Furthermore, the major disorganization and destruction observed within OE tissues induced by the 273 $ZnSO_4$ treatment was clearly identified, but no specific abnormality was observed in APP/PS1 mice. 274

The proposed study underlined that the OCT technique, though able to characterize macroscopic aspect of the OE, is still limited to observe changes at the cellular scale, especially in term of spatial resolution. When a recent study reinforces this conclusion (Ueda et al., 2019), some reported works have demonstrated, using more advanced OCT devices, that this technique allowed observing more structural details. For instance, in (Watanabe et al., 2011), authors highlighted layered organization of the rat olfactory epithelium. Recently, new generation of OCT systems, such as polarization sensitive OCT (PS-OCT) or microcontrast OCT (MC-OCT) are expected to offer a micrometer resolution optical investigation (i.e., 5 to 7 times better than our OCT system) as demonstrated in recent works dealing with the visualization of nerve fiber pathways in a rat's brain (Wang et al., 2014b,a).

Promising results were obtained using confocal microscopy technique. The latter outperforms the OCT since it can be used for visualization both the OE structural layered organization and axons bundles without the need of slicing or specific tissue labelling as usually performed in histology. The noninvasive manner of this technique and the fact that it did not require specific labelling of the tissue makes it a reliable candidate for in vivo investigation on patients. Millimeter confocal microscopy probe already exists on the market. Its future in vivo use could therefore be possible, for instance, when the microrobotic system under development within the NEMRO project will be finalized (Fig. 7).

291 One of the major challenges of the nasal cavity endoscopy is the early, sensitive and specific diagnosis of neurodegenerative diseases such as Alzheimer's disease. Both OCT and confocal microscopy are not 292 293 efficient in the visualization of other precursor signs such as Amyloid- β peptide deposits within the OE 294 tissues. In our study, we investigated the potential of the well-established CellVizio system that requires fluorescence to detect the presence of Amyloid- β peptides deposit on OE tissues. One of the arguments in 295 296 favor of the used of CellVizio probe is that it is available on different sizes ranging from a few hundred 297 micrometers to a few millimeters that offer spatial resolution between $1.4\mu m$ to $3.5\mu m$. In addition, depending on the considered probe, it is possible to visualize the tissue at different depths until $100\mu m$ 298 299 below the surface, i.e., able to observe independently different tissues layers.

Preliminary results have demonstrated that CellVizio technology allowed the visualization of the different 300 elements of the OE tissues. This technology could enable the identification of the presence of Amyloid- β 301 peptides deposits within the OE tissues. Indeed, we presumed that the green spots shown in Fig. 6C could 302 be Amyloid- β deposits given that the whole OE (not cut in 10m section) was stained by immersion with an 303 primary antibody targeting Amyloid- β peptides. However, further developments and improvements are 304 required to establish a more trivial and non-invasive tissues labelling procedure, particularly in case of in 305 vivo investigation on patients. Actually, a conceivable method for in vivo labelling tissues on patients could 306 be the delivery of fluorescent agent by spraying. 307

Besides Amyloid- β deposition, confocal microscopy technique demonstrated its ability to highlight 308 potential structural changes and morphological alterations within the OE tissues or in retina as recently 309 reported in the literature. Indeed, various studies in patients suffering from Alzheimer's disease as well as in 310 animal models reported that retinal structural deficits such as peripapillary atrophy, thinning of the macular 311 ganglion cell complex, axonal degeneration in the optic nerve, or cellular degeneration associated to visual 312 dysfunctions (Hart et al., 2016). It can be hypothesized that these structural deficits of the retina that occur 313 prior to the first signs of memory or motor loss in Alzheimer's patients, could be also identified within the 314 OE tissues, starting with neurofibrillary tangles (Talamo et al., 1989) or axonal degeneration (Kovacs et al., 315 1999). 316

Future works will focus on reproducing the described methods and results on human tissues. First, we will start with the evaluation of the insertion and navigation of such imaging tools on human cadavers. To do this, it is necessary to integrate the imaging tools into the robotic endoscopic system for further in vivo characterization of OE tissues. A 2:1 prototype of the robotic endonasal system (Fig. 7) is already developed and its functionalities are currently being tested on nasal phantoms. In the longer term, the developed robotic device system will serve as a safe intranasal navigation system without collisions with the nasal walls. If part of the OE is accessible in an almost straight line between the entrance of the nasal slots and the beginning of the OE, the rest of the tissues is unreachable. The flexible endonasal robot
could address this concern. Additionally, the robot has a free internal channel that will allow inserting the
characterization imaging system such as the CellVizio probe.



Figure 7. Illustration of the endonasal robotic concept under development for in vivo OE characterization (Chikhaoui et al., 2016)

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327 As a reminder, the objectives of this work was the evaluation of the capabilities of advanced imaging tools to highlight disorders that occur with the OE tissues. These disorders can be considered as early 328 signs of a neurodegenerative disease, a correlation that has been widely reported in the literature over the 329 last two decades. Today, Alzheimer disease can only be definitively diagnosed post-mortem thanks to a 330 histopathological examination or in the case where the progress of the disease is very significant. Currently, 331 the main diagnosis tools are the lumbar puncture and the scintigraphy. The study of the olfactory epithelium 332 tissues can provide Alzheimer's disease diagnosis, if not at an early stage, it can be at least a means of 333 establishing the disease (Godoy et al., 2019). 334

5 ADDITIONAL REQUIREMENTS

For additional requirements for specific article types and further information please refer to AuthorGuidelines.

CONFLICT OF INTEREST STATEMENT

The authors declare that the research was conducted in the absence of any commercial or financialrelationships that could be construed as a potential conflict of interest.

ETHICS STATEMENT

339 All animal use and care protocols were in accordance with institutional guidelines, and with the Directive

340 2010/63/EU of the European Parliament, and of the Council of 22 September 2010, on the protection of

341 animals used for scientific purposes.

AUTHOR CONTRIBUTIONS

- 342 All listed authors contributed substantially, directly and intellectually to the work described in this paper,
- 343 and approved it for publication.

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