

Article Laser Actuated Microgripper using Optimized Chevron-shaped Actuator

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- 1 Abstract: In this paper, we propose a laser actuated microgripper that can be activated remotely
- ² for micromanipulation applications. The gripper is based on an optothermally actuated polymeric
- ³ chevron-shaped structure coated with optimized metallic layers to enhance its optical absorbance.
- Gold is used as a metallic layer due to its good absorption of visible light. The thermal deformation
- 5 of the chevron-shaped actuator with metallic layers is first modeled to identify the parameters
- 6 affecting its behavior. Then, an optimal thickness of the metallic layers that allows the largest
- possible deformation is obtained and compared with simulation results. Next, microgrippers
- are fabricated using conventional photolithography and metal deposition techniques for further
 characterization. The experiments show that the microgripper can realize an opening of 40 µm,
- ³ characterization. The experiments show that the interographic can realize an opening of 40 μm,
- a response time of 60 ms, and a generated force in the order of hundreds of μN. Finally, a pick and-place experiment of 120 μm microbeads is conducted to confirm the performance of the
- ¹¹ and-place experiment of 120 µm microbeads is conducted to confirm the performance of the ¹² microgripper. The remote actuation and the simple fabrication and actuation of the proposed
- ¹² microgripper makes it a highly promising candidate to be utilized as a mobile microrobot for
- 11 1. 1. 1. 1. 1.
- 14 lab-on-chip applications.
- 15 Keywords: Microgripper; Micromanipulation; Optothermal actuation

16 1. Introduction

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The manipulation of micro-sized objects has drawn more attention in recent years to advance highly demanding domains such as microassembly and biomedicine [1–3]. Specifically, microgrippers are one of the widely used devices to handle microobjects [4–6]. At this scale, different actuation approaches, such as electric [7,8], thermal [9], magnetic [10] and optical [11], are used to control the motion of the microgripper, where piezoelectric and electrothermal actuation are most dominant in commercialized microgrippers. Because many microscale applications, especially biomedical applications, are conducted in closed environments, a remote actuation scheme is advantageous [12–14]. In fact, optothermal actuation, where light is utilized to generate heat at a specific location in an object, is one of the promising actuation approaches for microgrippers. Its remote and localized nature makes it a suitable candidate for mobile applications in closed environments [15]. Moreover, it allows simple integration of the microgripper in mobile microrobots, which are widely actuated by magnetic or acoustic fields, without affecting the actuation of the microrobot itself.

A number of works have utilized "the optothermal response to develop microactuators and microgrippers". In general, optothermal "microactuators and microgrippers are mainly implemented using smart material designs [16], or chevron-shaped actuators [17]. In smart material design, a photoresponsive material is mixed with a flexible material, e.g. polymers, to achieve a bending motion upon illumination [18]. These materials provide highly flexible motion that can be further controlled by patterning the

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mixed material through advanced techniques such as shape programming [19]. Nonethe-38 less, this comes at the cost of increased fabrication complexity. On the other hand, the 30 chevron-shaped actuators, which are commonly based on polymers and are fabricated 40 using conventional photolithographically techniques, offer an effective actuator that can 41 generate relatively large displacement without complex fabrication techniques, in con-42 trast to smart materials. Although the flexibility and range of motion of chevron-shaped 43 actuators is lower than their smart materials counterparts, they offer a comparatively 44 high generated force, which is critical for micromanipulation [20]. For instance, Elbuken 45 et al. [17] have developed a photothermally actuated microgripper fabricated with a single polymeric layer (SU-8) and based on a chevron-shaped actuator. The microgrip-47 per could be actuated remotely to realize an opening of 30 µm using a focused laser beam to heat up a connection spot between two beams in the chevron-shaped structure. 10 However, a common problem when utilizing the photothermic behavior of polymeric actuators is their low optical absorbance [21], which drastically reduces the overall 51 displacement of such actuators. Because chevron-shaped actuators can be fabricated 52 with common microelectromechanical systems (MEMS) fabrication techniques, a viable 53 workaround is to use metallic coating to enhance the optical absorbance. By using a metal with high optical absorbance, the overall deflection of the chevron-shaped actuator 55 can be increased. Moreover, the high absorbance of optical energy drastically enhances 66 the response speed of the actuator. Specifically, gold is a superior absorbent of visible 57 light and has shown high potential in optothermal actuation [22,23]. For example, gold 58 nanoparticles have been integrated in a tunable biopolymer material to facilitate its op-59 tothermal response [24]. Moreover, gold is a commonly available material in cleanrooms 60 with a well know deposition processes. Still, the integration of gold in microactuators 61 increases its fabrication complexity. In this paper, we propose a polymeric microgripper 62 utilizing a gold metallic coated chevron-shaped actuator that can be actuated remotely 63 with a laser. Our aim is to overcome the low optical absorbance limitation of polymers 64 by introducing a gold metallic layer with optimal thickness that would not affect the 65 flexibility of the polymer itself. The thickness of the metallic layer is optimized to realize 66 the largest possible opening of the microgripper. By virtue of the metallic layer, the proposed microgripper can realize large displacements and a fast response compared to 68 previously developed polymeric microgrippers. To our knowledge, this work is the first attempt to enhance the optothermal actuation of chevron-shaped microgrippers using 70 metallic coating. The untethered nature of laser actuation makes it possible to integrate the microgripper in a mobile microrobot in future work. 72

73 2. Microgripper Design, Optimization, and Fabrication

In this section, the microgripper design and the base material choice are first introduced. Next, the metal-coated chevron-shaped actuator, which is the main component of the microgripper, is optimized to realize relatively large deflections. Finally, the fabrication process of the microgripper is shown.

78 2.1. Design of Microgripper

The main component of the proposed microgripper is a chevron-shaped thermal 79 actuator that produces translational displacement when heated. The two beams of the 80 actuator, called "chevron beams", are connected to the body of the microgripper from 81 one end, acting as a fixed end, and to a common connection point, called "chevron 82 shuttle", acting as a free end, as shown in Figure 1(a). It is worth noting that it is 83 possible to add more pairs of chevron beams to the design as will be shown in the 84 experimental section. Upon heating the chevron shuttle using a focused laser beam, the heat is conducted through the chevron beams causing them to expand, creating a translational displacement at the shuttle, as shown in Figure 1(b). This displacement is 87 utilized to push the fingers of the microgripper, which are normally in a closed state, 88 further apart achieving an open state. Specifically, the normally closed state allows 89

- ⁹⁰ the microgripper to hold and move microobjects without being continuously heated
- ⁹¹ by the laser beam, which is preferable to reduce the amount of heat dissipated in the



⁹² surrounding environment.

Figure 1. (a) Schematic of the proposed microgripper. (b) Laser heating of the chevron-shaped actuator results in opening the microgripper. (c) Material structure of the microgripper. (d) Dimensions of the microgripper. Two possible designs with two chevron beams (n = 2) and four chevron beams (n = 4) are shown. All dimensions are in µm.

The material structure of the microgripper is shown in Figure 1(c). SU-8 resin was 93 chosen as the body material of the microgripper. The use of SU-8 offers a number of advantages in microfabrication and thermal actuation. Because SU-8 is a very common 95 material in MEMS manufacturing, its fabrication process is straightforward and it can be deposited in a thick layer (several ten microns). In addition, SU-8 is known to produce 97 relatively large displacements in response to temperature change owing to its high thermal expansion coefficient [25]. On the other hand, the use of SU-8 poses a number of 99 disadvantages especially in the case of optothermal actuation. Specifically, the thermal 100 conduction coefficient of SU-8 is low, which is both advantageous and disadvantageous. 101 In fact, when heating the chevron-shaped actuator with a laser, the low thermal con-102

duction coefficient of SU-8 drastically reduces the amount of heat conducted from the
heated actuator to the fingers of the microgripper. This is advantageous in biomedical
applications to prevent damage to the manipulated biological entities. However, the
disadvantage is the low temperature conduction from the heated shuttle to the beams
of the chevron-shaped actuator, which reduces its overall displacement. Moreover, the
transparent nature of SU-8 drastically reduces its optical absorbance; thus reducing its
deformation when heated using a laser beam.

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To compensate for the transparency of SU-8 and to enhance its optical energy 111 absorption, a thin layer of a high optical absorbance metal is selectively deposited on 112 the chevron-shaped actuator. The metallic layers are deposited on both sides of the 113 actuator with equal thicknesses to reduce the bimaterial effect. In fact, the thickness of 114 the metallic layer is a key parameter to achieve the largest possible deflection. On the 115 one hand, an excessively thick layer would increase the stiffness of the chevron-shaped 116 actuator reducing its deflection. On the other hand, an excessively thin layer would 117 suffer from low optical absorbance. Therefore, the thickness of the metallic layer should 118 be optimized for maximal possible deflection. The full design and dimension of the 119 microgripper are shown in Figure 1(d). The figure demonstrates the ability to vary 120 the number of chevron beams through two examples of chevron actuators having two 121 (n = 2), or four (n = 4) chevron beams. 122

2.2. Modeling and Optimization of Metal-coated Chevron-shaped Actuator

In order to optimize the design of the chevron-shaped actuator, a model should be first derived. Because the actuator is symmetrical on the yz-plane, a model of only half of the actuator cut in the yz-plane is derived for simplicity. A schematic of the deflection of a half chevron-shaped actuator upon heating is shown in Figure 2(a). The translational motion (δ) of the chevron shuttle can be estimated as a function of the variation in the length of the chevron beam (ΔL) as follows:

$$\delta = \sqrt{2L\Delta L + \Delta L^2 + L^2 \sin^2(\beta)} - L\sin(\beta)$$
(1)

$$\Delta L = \int_0^L T(x) \alpha \, \mathrm{d}x \tag{2}$$

where *L* is the length of the chevron beam, β is the angle of the chevron beam with 130 respect to the x-axis, T(x) is the temperature of the cross section of the chevron beam 131 located at x coordinate, and α is the thermal expansion coefficient. From the model, it 132 can be confirmed that the deflection of the chevron shuttle (δ) increases with decreasing 133 angle of the chevron beam (β). The temperature conduction along the chevron beam can 134 be modeled similar to the heat transfer from a fin by assuming that the temperature is constant over a small length dx as shown in Figure 2(b). The temperature conduction 136 should take into account the different thermal conductivity of the the SU-8 body and the 137 two metallic layers. The two metallic layers have equal thicknesses ($e_{m1} = e_{m2} = e_m$). 138



Figure 2. Modeling of the thermal deformation of a metal coated chevron-shaped actuator. (a) Schematic of the deflection of a half chevron-shaped actuator upon heating. (c) A sectional view of the chevron beam. (c) Effect of the thickness of the metallic layer on the length variation of the chevron beam. The blue dashed line and the red solid line show the model calculations and the simulation results, respectively. (d) Effect of adding metallic layers on the temperature gradient of the chevron actuator. The metallic layers thicknesses $e_{m1} = e_{m2} = e_m = 200$ nm. The red solid line and the red dashed line show the model calculations for the cases with and without metallic layers, respectively, and the blue line and the blue dashed line show the simulation results for the cases with and without metallic layers, respectively.

$$\frac{d^2T(x)}{dx^2} = h\frac{p}{\lambda A}(T(x) - T_{amb})$$
(3)

where *h* is the heat transfer coefficient of air, λ is the thermal conductivity of the chevron beam material, *p* is the perimeter of the chevron beam cross-section, *A* is the area of the chevron beam cross-section, and T_{amb} is the ambient temperature. By substituting the geometrical parameters of the chevron beam and the two different thermal conductivities of SU-8 and the metallic layers in equation (3) we can get:

$$\frac{d^2 T(x)}{dx^2} = h \frac{(2W + 4e_m + 2e_s)}{\lambda_s A_s + 2\lambda_m A_m} (T(x) - T_{amb})$$
(4)

where λ_s , λ_m are the thermal conductivities of SU-8 and the metallic layers, respectively, e_s , e_m are the thicknesses of SU-8 and the metallic layers, respectively, W is the width of the chevron beam, and A_s , A_m are the areas of the cross sections of the SU-8 layer and the metallic layers, respectively. The solution for equation (4) gives us the temperature profile along the length of the chevron beam as follows:

$$T(x) = B \exp(Dx) + C \exp(-Dx) + T_{amb}$$
(5)

$$D = \sqrt{\frac{h(2W + 4e_m + 2e_s)}{\lambda_s A_s + 2\lambda_m A_m}};$$
(6)

$$B = T_f - T_{amb} - \frac{T_i - T_{amb} + (T_{amb} - T_f) \exp(DL)}{\exp(-DL) - \exp(DL)};$$
(7)

$$C = T_f - B - T_{amb} \tag{8}$$

where T_i , T_f are the initial and final temperatures of the chevron beam. Finally, the length variation expressed in equation (2) can be rewritten as:

$$\Delta L = \int_0^L T(x) \alpha_{eq} \, \mathrm{d}x = \frac{\alpha_{eq}}{D} (B \exp(DL) - C \exp(-DL) - (B - C)) \tag{9}$$

$$\alpha_{eq} = \frac{A_s E_s \alpha_s + 2A_m E_m \alpha_m}{A_s E_s + 2A_m E_m} \tag{10}$$

where E_s , E_m are the Young's moduli of SU-8 and the metallic layers, respectively, and 151 α_s , α_m are the thermal expansion coefficients of SU-8 and the metallic layers, respectively. 152 Equation (9) gives a relation between the parameters of the chevron-shaped actuator 153 and its thermally induced length variation. Therefore, the effect of the thickness of the 154 metallic layer on the length variation can be estimated, as shown in Figure 2(c). The 155 figure includes the model calculations based on equation (9), shown in the blue dashed 156 line, and the simulation results using Comsol shown in the red solid line. It can be 15 confirmed from the figure that an optimal value for the thickness of the metallic layer, 158 which can generate the maximum length variation of the chevron-beam, can be obtained. This value was confirmed to be 200 nm and it will be used in subsequent sections. In 160 addition, the maximum opening of the microgripper can be controlled by varying the 161 metallic layer thickness, taking in mind that all other parameters affecting ΔL , such 162 as the dimensions of the chevron beams and the length of the microgripper's fingers, 163 are fixed. On the other hand, the temperature gradient along the chevron-beam can 164 be obtained using equation (5), as shown in Figure 2(d). The same equation can be used to verify the effectiveness of the metallic layer by verifying the effect of adding 166 a metallic layer on the temperature gradient. Two cases of chevron beams with and 167 without metallic layers are shown. Here, the optimal value of 200 nm for the thickness 168 of metallic layer is used. The figure includes the model calculations based on equation 169 (5) for the cases with and without metallic layers, shown in the red solid line and red 170 dashed line, respectively, and the simulation results using Comsol for the cases with 171 and without metallic layers, shown in the blue line and blue dashed line, respectively. 172 In the case of no metallic layer, the temperature exponentially drops along the length 173 of the chevron-beam, which reduces its overall length variation. On the other hand, a 174 linear drop in temperature along the length of the chevron-beam can be confirmed after 175 adding metallic layer, which shows the advantage of adding an optimized metallic layer 176 to the chevron-shaped actuator. 177

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179 2.3. Fabrication of Microgripper

The microgripper is fabricated using conventional photolithography and metal 180 deposition techniques. The process uses three different masks to construct the main 181 SU-8 body and metallic layers of the microgipper. The fabrication flowchart is shown in 182 Figure 3(a), and is described as follows: (1) an 800 nm sacrificial layer of aluminum (Al) 183 is deposited by sputtering on a silicon (Si) wafer. (2) a 350-nm thick layer of chromium 184 (Cr), a 200-nm thick layer of gold (Au), and a 45-nm thick layer of Cr are deposited by sputtering, respectively. The chromium layers are added to enhance the adhesion 186 between metal-metal layers and metal-polymer layers. (3) the first photolithography 187 process using the first mask (mask A) is conducted with positive photoresist (S1813) 188

to shape the lower metallic layers. (4) wet etching of Cr followed by wet etching of 189 Au are conducted for 30 sec and 2 min, respectively. (5) the photoresist is removed by 190 acetone. (6) a 50 µm-thick layer of SU-8 is deposited using spin coating. Two-steps spin 191 coating is used with speeds of 500 rpm for 30 sec and 2500 rpm for 30 sec, respectively. 192 (7) the second photolithography process using the second mask (mask B) is conducted 193 to shape the SU-8 layer. (8) a 45-nm thick layer of Cr and a 200-nm thick layer of Au are 194 deposited by sputtering, respectively. (9) the third photolithography process using the 195 third mask (mask C) is conducted with positive photoresist (S1813) to shape the upper 196 metallic layers. It is worth noting that mask C is similar to mask A but with enlarged thin 197 parts of the microgripper, such as the chevron beams, to simplify the alignment process. 198 (10) wet etching of Au followed by wet etching of Cr are conducted for 2 min and 5 1 9 9 min, respectively. (11) the photoresist is removed by acetone. (12) the microgrippers are 200 released by wet etching of Al followed by wet etching of Cr. The etching times in this 201 step were determined visually until the removal of the Al and Cr layers are confirmed. 202 An example of a fabricated microgripper is shown in Figure 3(b). 203



Figure 3. (a) Flowchart of the microgripper fabrication process. (1) Deposition of Al sacrificial layer. (2) Deposition of lower metallic layers. (3) First photolithography using mask A to shape the lower metallic layers. (4) Wet etching of lower metallic layers. (5) Removal of photoresist using acetone. (6) Spin coating of SU-8. (7) Second photolithography using mask B to shape the main body of the microgripper. (8) Deposition of upper metallic layers. (9) Third photolithography using mask C to shape the upper metallic layers. (10) Wet etching of upper metallic layers. (11) Removal of photoresist using acetone. (12) Wet etching of Al sacrificial layer and Cr layer to release the structures. (b) Image of a fabricated microgripper.

204 3. Experiments

In this section, the behavior of the fabricated microgrippers is characterized. The optothermal response using laser actuation and the generated force of the microgrippers are evaluated. Subsequently, the functionality of the microgrippers is confirmed through a micromanipulation experiment of microbeads.

209 3.1. Microgripper Actuation and Response

In this section, the laser actuation of the microgripper by utilizing its optothermal response is confirmed. The experimental setup for laser actuation of the microgripper is shown in Figure 4(a). The system mainly consists of a CMOS camera (Allied Vision Inc.) attached to a microscope to visualize and record the actuation of the microgripper. In addition, a continuous wave (CW) laser (Oxxius Inc.) with a power of 53.3 mW and a wavelength of 532.1 nm was used as a laser source. The laser beam was focused using an $20 \times$ objective lens (Nikon Inc.), where the focused laser spot size was approximately $300 \mu m$.

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Figure 4(b) shows the actuation of the microgripper. The microgripper is initially in 219 a closed state without any laser heating. Upon laser heating of the chevron shuttle, the 220 open state of the microgripper can be realized. The initial gap between the two fingers 221 of the microgripper is approximately 100 µm (close) and then increased to 140 µm (open) 222 by laser heating. The achieved displacement of 40 μ m is approximately 1.3 times higher 223 compared to similar designs without metallic layers deposition [17]. Figure 4(c) shows 224 the step response of the microgripper. From the response, a comparatively fast response 225 time, i.e. the time to reach 50% of the steady-state opening value of the microgripper, of 226 approximately 60 ms is confirmed, which is 23 times faster compared to similar designs 227 without metallic layers deposition [17]. Moreover, to confirm the frequency response of the microgripper, the change in magnitude of the opening of the microgripper in 229 response to a frequency sweep is confirmed. Figure 4(d) shows the bode magnitude 230 plot of the microgripper response. The frequency sweep is achieved using a square 231 wave supplied to a tip/tilt mirror (Physics Instruments Inc.) to steer the laser beam 232 to and away from the chevron shuttle of the microgripper with frequencies ranging 233 from 1 to 20 Hz. As a result, the opening of the microgripper varied according to the 234 applied frequency. From the frequency response, a cut-off frequency, i.e. the frequency 235 where the magnitude reaches -3 dB value, is confirmed to be approximately 5.5 Hz. This 236 frequency modulated response can be used to apply a periodic force to grabbed cells 237 or microobjects in future work. These results clearly show the advantage of utilizing 238 metallic layer deposition to enhance optothermal actuation. 239



Figure 4. Laser actuation of the microgripper. (**a**) Experimental setup. (**b**) Experimental images showing the close and open states of the microgripper. (**c**) Step response of the microgripper. (**d**) Bode magnitude plot of the microgripper using a frequency sweep from 1 to 20 Hz

240 3.2. Generated Force

For micromanipulation applications, the gripping force generated by the micro-241 gripper should be suitable to firmly hold microobjects. Therefore, the force generated 242 by the fingers of the microgripper is investigated. However, measuring the exact force 243 generated by the two fingers connected to the chevron-shaped actuator proves to be chal-244 lenging, where a force sensing device should be placed between the fingers. Therefore, the stiffness of only one arm connected to the chevron-shaped actuator is confirmed, 246 which gives a good estimate of the order of magnitude of the generated force. In fact, 247 there are a number of design parameters that affects the generated force of the microgrip-248 per [17]. In this work, we investigate the effect of two parameters, namely the width of 249 the chevron beams (W) and the number of chevron beams (n). The measurement setup 250 is shown in Figure 5(a). A force sensor (Femtotools inc.) with a resolution of 0.05 μ N 251 and a range of $1000 \,\mu\text{N}$ is attached to a motorized x stage (Physik Instrumente Inc.) with 252 a positioning accuracy of $0.05 \,\mu\text{m}$ and a range of 25 mm. The microgripper is attached to 253 a stationary holder to have the same vertical position (z-axis) as the force sensor. The 254 alignment between the probe of the force sensor and the finger of the microgripper is 255 confirmed visually as shown in 5(b). Subsequently, the motorized x stage is moved for 256 20 µm to allow the probe to push the finger of the microgripper. A data acquisition 257 routine is initiated simultaneously to record the position of the x stage and the force 258 sensor data. Consequently, a linear relation between the force and the stage displacement 259 can be obtained using linear regression, where the stiffness is confirmed as the slope 260 of the plotted curve (please refer to Figure S1 in supplementary materials). It is worth 261 noting that the force is applied along the x-axis; thus only one component of the force is 262 present. Indeed, each finger of the microgripper has two degrees of freedom (x-axis and 263 y-axis) and it is more accurate to describe the stiffness in a matrix form to account for the 264 coupling stiffnesses. However, this increases the complexity of the force measurement 265 experiment and the analysis. Therefore, as the aim is to get an estimate of the order of 266 magnitude of the force applied by the microgripper to confirm its ability to manipulate 267 microobjects, a simple unidirectional force estimation is sufficient. A more rigorous force 268

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269 measurement will be planned in future work.

Figure 5(c-d) shows the experimental results, shown in blue bars, and simulation 271 results using Comsol, shown in brow bars, of the stiffness of one microgripper finger. 272 For the simulation, the commonly used value of 4 GPa for the Young's modulus of SU-8 273 is used [26]. The experimental measurements are repeated four times on four different 274 microgrippers for each plotted bar, where the error bars indicate the mean value and the 275 standard error of the measurements. Figure 5(c) shows the effect of the chevron beam 276 width on the stiffness. Two width values of 10 µm and 15 µm are investigated, where 277 the number of chevron beams is fixed to n = 2. it can be seen from the results that the 278 width of the chevron beam had a noticeable effect on the stiffness, where an increase in 279 stiffness of approximately 23% can be confirmed. Figures 5(d) shows the effect of the 280 number of chevron beams on the stiffness. Two cases with chevron-shaped actuators 281 having two, and four beams, respectively, where investigated, where the width of the 282 chevron beams are fixed to $W = 15 \,\mu\text{m}$. In this case, an increase of approximately 6% in 283 the stiffness when doubling the number of chevron beams can be confirmed. It can be 28 concluded from the figures that the impact on the stiffness is higher when increasing 285 the width of the chevron beams compared to increasing the number of chevron beams. 286 Finally, it can be noticed that the experimental results and the simulation results differ 287 significantly. This can be due to the difference in the Young's modulus value between the simulation and experiments, since the physical parameters of SU-8 can change 289 according to the fabrication process. To confirm this effect, the Young's modulus was 290 increased in the simulation from 4 GPa to 8 GPa and the resulting stiffnesses are plotted 291 in Figures 5(c, d) shown in orange columns. It is found that by increasing the Young's modulus, stiffness values that are much closer to the experimental results are obtained. 293 The residual difference between the experimental and simulation results can be caused 294 by the inaccuracies in the fabrication process, such as a drift in the width and thickness 295 of the chevron beams, or the alignment between the SU-8 layer and the gold layer. Still, more investigation on the stiffness of SU-8 using our fabrication process will be planned 297 in future work. Overall, the experimental results serve as a good indicator for the order 298 of magnitude of the generated force, which is in the order of hundreds of micronewtons. 299 This force range is similar to many commercial microgrippers and is suitable for a variety 300 of micromanipulation applications [27]. 301





302 3.3. Application to Micromanipulation

To confirm the performance of the microgripper in micromanipulation applications, 303 a pick-and-place experiment on a 120-µm diameter microbead is performed. The micro-304 gripper incorporates two pairs of chevron beams (four beams) to enhance the gripping 305 force. The microbead is put on a cover glass and actuated using an XYZ piezoelectric 306 motorized stage (Physik Instrumente Inc.), whereas the microgripper is attached to a 307 stationary holder, as shown in Figure 6(a). The stationary position of the microgripper 308 allows the initiation of open/close gripping motion at any instance during the experi-309 ment. Figure 6(b) demonstrate the results of the pick-and-place experiment. First, the 310 microbead is brought to the same vertical position (z-axis) as the microgripper, where 311 the microgripper is in a closed state with no application of laser heating (Figure 6(b-1)). 312 Next, the microgripper is switched to an open state by initiating the laser heating, and 313 the microbead is actuated and positioned between the arms of the gripper (6(b-2)). Con-314 sequently, the microgripper is returned to the closed state by switching off the laser and 315 the microbead is firmly held and actuated away from the coverglass (6(b-3, b-4)). Finally, 316 the opposite maneuver is repeated to place the microbead on the cover glass again (6(b-5, 317 b-6)). The successful manipulation of the microbead demonstrates the potential of the 318 proposed microgripper to be used in micromanipulation and biomedical applications. 319 320

To get a better conclusion on the weights of objects that can be manipulated using 321 the microgripper, the weight of the manipulated microbead is estimated analytically. 322 As the volume and density of the microbead are known, the weight is estimated to be 323 approximately 1 µg. In fact, many microobjects fall in this range of size and density. 324 Specifically, biological cells are mostly equal or smaller than 120 µm in diameter with 325 lower densities than glass. Therefore, the proposed microgripper is expected to be able 326 to handle a large variety of microobjects including cells. The maximum weight limitation 327 of the gripped object is mainly affected by the static friction force generated by the 328 normal force applied on the object. This requires the estimation of the static friction 329 coefficient, which is challenging to acquire at this small scale. Nonetheless, the generated 330 force of the microgripper in the range of hundreds of µN is similar to many commercial 331 microgrippers and is suitable for many micromanipulation applications. 332



Figure 6. Pick-and-place of a microbead. (a) Experimental setup. (b) Snapshots of the experiment showing the successful pick-and-place of a 120-µm diameter microbead on a cover glass. See attached video.

333 4. Conclusions

In this article, we proposed a laser actuated microgripper based on a metal-coated 334 chevron-shaped actuator for micromanipulation applications. The thermomechanical 335 model of the metal-coated microgripper was established to identify the parameters affect-336 ing its thermal deflection. Consequently, an optimization process was conducted to find 337 the optimal thickness of the metallic layer that achieves the largest possible deflection. 338 Microgrippers were fabricated with SU-8 resin and gold coating using conventional 339 photolithography and metal deposition techniques. The optothermal response and the 340 generated force of the microgrippers were verified through characterization experiments. 341 The microgrippers could realize a relatively large opening of 40 µm with a relatively fast 342 response time of 60 ms. Finally, the functionality of the microgripper was demonstrated 343

- through a successful pick-and-place experiment of a microbead.
- 345

Because this kind of remotely actuated microgrippers are highly promising for 346 mobile microrobotic application, the future direction of this work is to utilize the micro-347 gripper as a mobile microrobot to be deployed in lab-on-chip applications. To achieve 348 this goal, the behavior of the optothermal actuation in liquid needs to be verified first. In 349 addition, a remote actuation scheme, such as magnetic or acoustic actuation, to control 350 the position of the microgripper needs to be integrated and tested. Moreover, as the 351 fluidic flows generated by objects inside microfluids are significant and can affect the 352 position of target microobjects, it is desirable to reduced the footprint of the microgripper 353 by fabricating a miniaturized version. In this case, the size of the laser spot needs to be 354

- adjusted to be compatible with the miniaturized chevron-shaped actuator.
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References

- 1. Zhang, Z.; Wang, X.; Liu, J.; Dai, C.; Sun, Y. Robotic micromanipulation: Fundamentals and applications. *Annual Review of Control, Robotics, and Autonomous Systems* **2019**, *2*, 181–203.
- 2. Li, X.; Fukuda, T. Magnetically guided micromanipulation of magnetic microrobots for accurate creation of artistic patterns in liquid environment. *Micromachines* **2020**, *11*, 697.
- Jing, W.; Chowdhury, S.; Guix, M.; Wang, J.; An, Z.; Johnson, B.V.; Cappelleri, D.J. A microforce-sensing mobile microrobot for automated micromanipulation tasks. *IEEE Transactions on Automation Science and Engineering* 2018, 16, 518–530.
- 4. Gursky, B.; Bütefisch, S.; Leester-Schädel, M.; Li, K.; Matheis, B.; Dietzel, A. A disposable pneumatic microgripper for cell manipulation with image-based force sensing. *Micromachines* **2019**, *10*, 707.
- 5. Power, M.; Thompson, A.J.; Anastasova, S.; Yang, G.Z. A monolithic force-sensitive 3D microgripper fabricated on the tip of an optical fiber using 2-photon polymerization. *Small* **2018**, *14*, 1703964.
- 6. Yin, C.; Wei, F.; Zhan, Z.; Zheng, J.; Yao, L.; Yang, W.; Li, M. Untethered microgripper-the dexterous hand at microscale. *Biomedical microdevices* **2019**, *21*, 82.
- Velosa-Moncada, L.A.; Aguilera-Cortés, L.A.; González-Palacios, M.A.; Raskin, J.P.; Herrera-May, A.L. Design of a novel MEMS microgripper with rotatory electrostatic comb-drive actuators for biomedical applications. *Sensors* 2018, 18, 1664.
- 8. Lyu, Z.; Xu, Q. Recent design and development of piezoelectric-actuated compliant microgrippers: A review. *Sensors and Actuators A: Physical* **2021**, 331, 113002.
- 9. Cauchi, M.; Grech, I.; Mallia, B.; Mollicone, P.; Sammut, N. The effects of cold arm width and metal deposition on the performance of a U-beam electrothermal MEMS microgripper for biomedical applications. *Micromachines* **2019**, *10*, 167.
- 10. Kuo, J.C.; Huang, H.W.; Tung, S.W.; Yang, Y.J. A hydrogel-based intravascular microgripper manipulated using magnetic fields. *Sensors and Actuators A: Physical* **2014**, *211*, 121–130.
- 11. Pevec, S.; Donlagic, D. Optically controlled fiber-optic micro-gripper for sub-millimeter objects. Optics letters 2019, 44, 2177–2180.
- 12. Ahmad, B.; Gauthier, M.; Laurent, G.J.; Bolopion, A. Mobile Microrobots for In Vitro Biomedical Applications: A Survey. *IEEE Transactions on Robotics* **2021**. doi:10.1109/TRO.2021.3085245.
- 13. Feng, L.; Hagiwara, M.; Ichikawa, A.; Arai, F. On-chip enucleation of bovine oocytes using microrobot-assisted flow-speed control. *Micromachines* **2013**, *4*, 272–285.
- 14. Ahmad, B.; Kawahara, T.; Yasuda, T.; Arai, F. Microrobotic platform for mechanical stimulation of swimming microorganism on a chip. IEEE/RSJ International Conference on Intelligent Robots and Systems. Chicago, IL USA, 2014, pp. 4680–4685.
- 15. Villangca, M.J.; Palima, D.; Banas, A.R.; Glückstad, J. Light-driven micro-tool equipped with a syringe function. *Light: Science & Applications* **2016**, *5*, e16148.
- 16. Huang, C.; Lv, J.a.; Tian, X.; Wang, Y.; Liu, J.; Yu, Y. A remotely driven and controlled micro-gripper fabricated from light-induced deformation smart material. *Smart Materials and Structures* **2016**, *25*, 095009.

- 17. Elbuken, C.; Khamesee, M.B.; Yavuz, M. Design and implementation of a micromanipulation system using a magnetically levitated MEMS robot. *IEEE/ASME Transactions on Mechatronics* **2009**, *14*, 434–445.
- 18. Lu, X.; Zhang, H.; Fei, G.; Yu, B.; Tong, X.; Xia, H.; Zhao, Y. Liquid-crystalline dynamic networks doped with gold nanorods showing enhanced photocontrol of actuation. *Advanced Materials* **2018**, *30*, 1706597.
- 19. Lahikainen, M.; Zeng, H.; Priimagi, A. Reconfigurable photoactuator through synergistic use of photochemical and photothermal effects. *Nature communications* **2018**, *9*, 1–8.
- 20. Shivhare, P.; Uma, G.; Umapathy, M. Design enhancement of a chevron electrothermally actuated microgripper for improved gripping performance. *Microsystem Technologies* **2016**, *22*, 2623–2631.
- Sharif, M.; Pourabbas, B.; Sangermano, M.; Sadeghi Moghadam, F.; Mohammadi, M.; Roppolo, I.; Fazli, A. The effect of graphene oxide on UV curing kinetics and properties of SU8 nanocomposites. *Polymer International* 2017, 66, 405–417.
- Ge, F.; Lu, X.; Xiang, J.; Tong, X.; Zhao, Y. An optical actuator based on gold-nanoparticle-containing temperature-memory semicrystalline polymers. *Angewandte Chemie* 2017, 129, 6222–6226.
- Bagheri, M.; Chae, I.; Lee, D.; Kim, S.; Thundat, T. Selective detection of physisorbed hydrocarbons using photothermal cantilever deflection spectroscopy. *Sensors and Actuators B: Chemical* 2014, 191, 765–769.
- 24. Wang, Y.; Li, M.; Chang, J.K.; Aurelio, D.; Li, W.; Kim, B.J.; Kim, J.H.; Liscidini, M.; Rogers, J.A.; Omenetto, F.G. Lightactivated shape morphing and light-tracking materials using biopolymer-based programmable photonic nanostructures. *Nature communications* **2021**, *12*, 1–9.
- 25. Sangermano, M.; Calvara, L.; Chiavazzo, E.; Ventola, L.; Asinari, P.; Mittal, V.; Rizzoli, R.; Ortolani, L.; Morandi, V. Enhancement of electrical and thermal conductivity of Su-8 photocrosslinked coatings containing graphene. *Progress in Organic Coatings* **2015**, *86*, 143–146.
- Xu, T.; Yoo, J.H.; Babu, S.; Roy, S.; Lee, J.B.; Lu, H. Characterization of the mechanical behavior of SU-8 at microscale by viscoelastic analysis. *Journal of Micromechanics and Microengineering* 2016, 26, 105001.
- Kim, K.; Liu, X.; Zhang, Y.; Sun, Y. Micronewton force-controlled manipulation of biomaterials using a monolithic MEMS microgripper with two-axis force feedback. IEEE International Conference on Robotics and Automation. Pasadena, CA USA, 2008, pp. 3100–3105.