

# 1 Atomic force microscopy characterization of polyethylene 2 terephthalate grafting with poly(styrene sulfonate)

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20

## 21 Abstract

22 Polyethylene terephthalate (PET) is widely used to elaborate biomaterials and medical  
23 devices in particular for long-term implant applications but tuning their surface properties  
24 remains challenging. We investigate surface functionalization by grafting poly(sodium 4-  
25 styrene sulfonate, PNaSS) with the aim of enhancing protein adhesion and cellular activity.

26 Elucidating the topography and molecular level organization of the modified surfaces is  
27 important for understanding and predicting biological activity. In this work, we explore  
28 several grafting methods including thermal grafting, thermal grafting in the presence of  
29 Mohr's salt, and UV activation. We characterize the different surfaces obtained using atomic  
30 force microscopy (AFM), contact angle (CA), and X-ray photoelectron spectroscopy (XPS). We  
31 observe an increase in the percentage of sulfur atoms (XPS) that correlates with changes in  
32 (CA), and we identify by AFM characteristic features, which we interpret as patches of  
33 polymers on the PET surfaces. This work demonstrates tuning of biomaterials surface by  
34 functionalization and illustrates the capability of atomic force microscopy to provide insights  
35 into the spatial organization of the grafted polymer.

36 **Keywords:** Peakforce Quantitative Nano-mechanical Properties (PF-QNM); Polyelectrolyte  
37 brushes; Polyethylene Terephthalate (PET), Poly(sodium 4-styrene sulfonate (PNaSS)

38

## 39 1. Introduction

40 Polyesters, in particular polyethylene terephthalate (PET), are used extensively in medical  
41 devices. Surface functionalization is often required to improve biological properties. Poly  
42 (sodium 4-styrene sulfonate) (PNaSS) is a strong polyelectrolyte, which has been proposed  
43 for the control of biological and biophysical properties including enhancing cell adhesion,  
44 spreading, and proliferation, thus improving bone tissue response[1,2], fibroblast behavior  
45 for reconstructing injured ligament and wound healing[2–5], antibacterial infection[6] and  
46 biocompatible surface[5,7]. PNaSS enhances the biological properties of PNaSS-grafted  
47 surfaces: the mechanism at the origin of this activity involves specific interactions between  
48 adsorbed binding proteins (fibronectin, FN) on functionalized surfaces and integrin at the cell  
49 membrane[1,2]. Briefly, the presence of sulfonate groups allows improving cell adhesion,  
50 proliferation, differentiation and/or biointegration in surrounding tissues when implanted in  
51 vivo[1]. This has been shown in vitro with different types of cells (fibroblast, endothelial cell,  
52 and osteoblast) and in vivo in the case of PNaSS-grafted titanium, PET and PCL implants.  
53 PNaSS immobilized on different materials such as titanium[1,8], polyethylene terephthalate  
54 (PET)[2,3], nanoparticle[5,9,10] or polycaprolactone (PCL) has been reported.

55 Several surface functionalization methods with poly(styrene sulfonate) have been proposed,  
56 e.g. sulfonation polystyrene brush [10,11] and grafting methods[12–14]. Among those,  
57 “grafting-from” has the advantage of being a scalable approach to the modification of  
58 interfacial properties through immobilizing the functional groups on the substrate by covalent  
59 bonding. The “grafting from” method starts with activation of the surface via plasma[15], UV  
60 irradiation[7,16], heating[14,18], in the presence of CuBr<sub>2</sub>[18–20], or Mohr's salt[13,14].

61 In this work, we activate PET surfaces by ozonation, a method convenient for materials with  
62 complex geometries such as implants[21]. Ozonation generates peroxide groups which  
63 decompose upon heating and UV irradiation[14,22,27] to generate radicals on PET; NaSS  
64 polymerizes from these active sites. The mechanism can be described as: the peroxides after  
65 decomposition form two types of free radicals, •OH and O•, and then C• (carbonyl)  
66 radicals[21] on the polymer chains. Free radicals •OH can be consumed by Fe<sup>2+</sup> in Mohr’s salt,  
67 thus reducing homopolymerization and promoting grafting[14,23,24].

68 Previous studies examined the effect of the graft PNaSS on the interaction of the modified  
69 surfaces with biological molecules yet the characterization of the grafted layer is often  
70 limited. Here, we investigate the topography of grafted polymers by atomic force microscopy  
71 (AFM) complemented by XPS and contact angle measurements.

72

## 73 **2. Materials and Methods**

### 74 **2.1. Materials**

75 Sodium 4- styrene sulfonate (NaSS), phosphate buffer saline (PBS), and Mohr's salt were  
76 purchased from Sigma Aldrich. Polyethylene terephthalate (PET) (0.25 mm, biaxially oriented  
77 plate) was purchased from Goodfellow (Paris, France). Ethanol absolute was from Fisher.

#### 78 **2.1.1. PET preparation:**

79 PET plate was cut into small squared pieces (1 cm × 1 cm). The surface was cleaned in an  
80 ultrasonic bath with ultrapure water, acetone, and ethanol for 10 min respectively. The  
81 samples were dried under vacuum for 2 h and stored at 4°C until use.

#### 82 **2.1.2. Monomer purification:**

83 The purification of NaSS was described [14,17,25] 90 g of NaSS was dissolved in 1.6 L of  
84 ethanol: distilled water (9:1, v/v) by stirring 12 h at 70°C. Thereafter, the solution was filtered  
85 by vacuum filtration. The filtered solution was kept at 4°C during 24 h for recrystallization.  
86 Recrystallized monomer was collected by vacuum filtration and was dried in vacuum at 30°C  
87 for 6 h. Finally, the product was kept at 4°C, away from the light.

88

## 89 **2.2. Functionalization of polyester surfaces by PNaSS (“grafting from”)**

### 90 **2.2.1. Activating the surfaces by ozonation**

91 The functionalization of polyesters by PNaSS includes two main steps: ozonation and grafting  
92 (Scheme 1). In the first step, the polymer surfaces were activated by ozonation using ozone  
93 generator BMT 802N. 6 PET plates were ozonized into 100 mL distilled water by introducing  
94 ozone flow (0.6 bars, 100 mL/min) for 20 min for PET at 30° C.[14] Ozonized samples were  
95 quickly transferred from the ozonation reactor to the degassed NaSS solution (0.7 mol/L) for  
96 grafting.

### 97 **2.2.2. Grafting PNaSS from PET substrate**

98 After activation by ozonation, PNaSS was polymerized from the activated sites (Scheme 1).  
99 For determining the influence of ozonation on the surface, non-grafted-ozonized polymer or  
100 ozonized PET without grafting was used as a reference. Non-grafted-ozonized PET was  
101 prepared by ozonation of a PET plate for 20 min at 30°C.

### 102 **Thermal radical polymerization (method 1 and 2):**

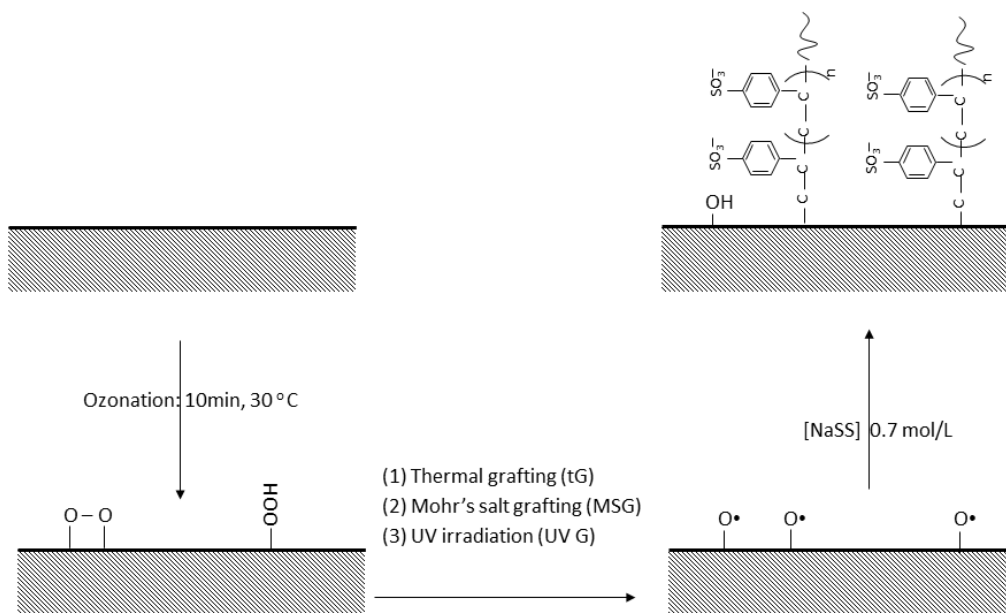
103 **Method 1 - Thermal grafting (TG)[13,14].** 6 ozonized PET plates were transferred into 60 mL  
104 of degassed NaSS (0.7 mol/L) solution and heated for 1 h at 75°C. Peroxide decomposition  
105 generates the radicals on the surface for initiating PNaSS polymerization.

106 **Method 2-Thermal grafting in the presence of Mohr's salt (MSG).** 6 ozonized PET plates were  
107 transferred into 60 mL degassed mixture solution of NaSS (9 g, 0.7 mol/L) and Mohr's salt (60  
108 mg, 0.1 %, w/v) and heated to 75°C for 1 h. Mohr's salt provides Fe(II) ions that increases  
109 significantly the grafting efficiency[14].

### 110 **Photoinitiated free radical polymerization (method 3):**

111 **Method 3-UV irradiation (UVG)**[22]. Peroxides were decomposed by UV irradiation. 6 PET  
112 plates were transferred into 60 mL of degassed NaSS solution (9 g, 0.7 mol/L). The solution  
113 was irradiated by UV light for 30 min (lamp UV-Omicure, 254 nm, 10 W/cm<sup>2</sup>) at 25°C under  
114 stirring.

115 After polymerization via either of the three methods above, free homopolymer, oligomer,  
116 and monomer were removed from the grafted samples under stirring in double distilled water  
117 for at least 48 h. The washing solution was tested by UV-vis at 360 nm to check for the  
118 presence of any residue of free PNaSS (homopolymer and oligomer). Samples were finally  
119 dried under vacuum and kept at 4°C, away from the light before use.



121 **Scheme 1. Grafting PNaSS from polyester surfaces by ozonation and radical polymerization**

122

### 123 2.3. Surface characterization

124 **X-ray photoelectron spectroscopy analysis (XPS).** X-ray photoelectron spectroscopy analysis  
125 (XPS) (from Omicron Argus spectrometer, Germany) was performed using a monochromated  
126 AlK $\alpha$  radiation source ( $h\nu = 1486.6$  eV) working at an electron beam power of 300 W with 90°  
127 of takeoff angle of photoelectrons emission, under ultra-high vacuum ( $\leq 10^{-10}$  Torr). Spectra  
128 were recorded at pass energy of 100 eV for the survey spectrum and pass energy of 20 eV for  
129 the high-resolution regions. Binding energies were calibrated against the C1s binding energy

130 of aliphatic carbon atoms at 284.8 eV. Spectral deconvolution was carried out using Casa XPS  
131 v.2.3.15 software (Casa Software Ltd, UK). All samples were dry films.

132 The equivalent thickness probed by XPS is estimated to be close to  $3\lambda = 10$  nm representing  
133 95% of the signal,  $\lambda$  being the inelastic mean free path of electrons from the PET substrate in  
134 the organic PNaSS film; for electrons having a kinetic energy around 1200 eV (from the C1s  
135 atomic level),  $\lambda$  is estimated to be equal to 3.23 nm.<sup>1</sup>

136 The estimated thickness ( $d$ ) of PNaSS on top of PET can then be calculated using the following  
137 formula:

$$138 \quad \frac{I_{S2p}}{I_{C1s\ 284\ eV}} = \frac{\rho_{PNaSS} M_{ET} \sigma_{S2p} T_{S2p} \lambda_{S2p}^{PNaSS} \left(1 - \exp\left(\frac{-d}{\lambda_{S2p}^{PNaSS} \sin(\theta)}\right)\right)}{\rho_{PET} M_{NaSS} \sigma_{C1s} T_{C1s} \lambda_{C1s}^{PET} \left(\frac{-d}{\lambda_{C1s}^{PNaSS} \sin(\theta)}\right)}$$

139  
140 Wherein:  $\theta$  is the photoelectron collection angle. TC1s and TS2p are the relative sensitivity  
141 factors of C and S, respectively, provided by the spectrometer manufacturer. The Scofield  
142 photoionization cross-sections  $\sigma$  are equal to 1 for C 1s and 1.44 for S2p.<sup>2</sup>  $\lambda_x y$  is the inelastic  
143 mean free paths of electrons  $x$  in the matrix  $y$ . They were calculated using the Quases program  
144 (QUASES-IMFP-TPP2M Ver.3.0) based on the TPP2M formula.  $\rho_{PNaSS}$  and  $\rho_{PET}$  are the  
145 density of PNaSS and PET, respectively.  $M_{NaSS}$  and  $M_{ET}$  are the molecular weight of NaSS  
146 (sodium styrene sulfonate) and ET (ethylene terephthalate), respectively.

147

148 **Contact angle.** DSA10 contact angle system from KRUSS GmbH was used to measure the  
149 surface tension by the sessile drop technique. Two solvents: water (polar), and  
150 diiodomethane (unpolar) (2  $\mu$ L, 25°C, 8s) were used. The surface tension of polymer ( $\gamma_s$ ) was  
151 calculated by Young-Dupre and Fowker's equation[26].

152 **Atomic Force Microscopy.** Atomic force microscope (AFM) multimode-8 from Bruker was  
153 used. AFM scans were carried out in air using Scanasyst probe (ScanAsyst cantilever (Silicon

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<sup>1</sup> Tanuma, S.; Powell, C. J.; Penn, D. R. Calculation of electron inelastic mean free paths (IMFPs) VII. Reliability of the TPP-2M IMFP predictive equation. *Surf. Interface Anal.* 2003, 35, 268–275.

<sup>2</sup> Scofield J (1976) Hartree–Slater subshell photoionization cross-sections at 1254 and 1487 eV. *J Electron Spectrosc Relat Phenom* 8(2):129–37

154 Nitride), triangular, reflective aluminium, symmetric tip with radius  $\leq 10$  nm,  $f_0$ : 70 KHz, spring  
155 constant:  $\sim 0.4$  N/m), scan rate 1 Hz, at different scan sizes:  $500\text{ nm} \times 500\text{ nm}$ ,  $2\ \mu\text{m} \times 2\ \mu\text{m}$   
156 ( $3$  samples). The absolute calibration was performed for each cantilever: Deflection Sensitive,  
157 Spring Constant ( $\sim 0.4$  N/m) using Thermal Tuning and Lorentzian fitting (air), and Tip Radius  
158 by Tip Qualification on Titanium roughness sample for PeakForce QNM (from BRUKER).  
159 Samples were dried in vacuum chamber in  $4$  h before scanning. Scanning was performed in  
160 the room conditions.  $3$  independent surfaces in the same grafting conditions were analyzed.  
161 The roughness ( $R_a$ ) was measured on  $3$  points/surface.

162 Nano-Scope Analysis v.1.5, Image-J and AtomicJ software[27] were used for image analysis.  
163 Surface mechanical properties was measured by Peakforce Quantitative Nano-mechanical  
164 Properties (PF-QNM) program[28]. When numbers of samples are indicated, they refer to  
165 independent experiments (from sample preparation).

166

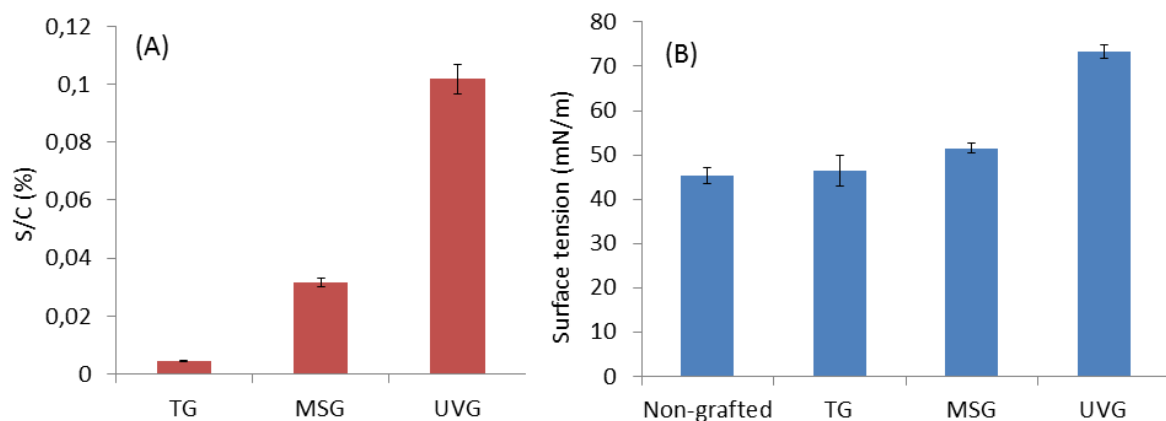
### 167 **3. Results**

#### 168 **3.1. Surface characterization**

169 As a NaSS unit contains one atom of sulfur, the surface density of grafted PNaSS can be  
170 estimated based on the percentage of sulfur atoms in the elementary composition using XPS.  
171 Sulfur was not detected on the non-grafted-ozonized PET surfaces, but the S2p peak was  
172 visible ( $165 - 170$  eV)[29] on the  $4$  grafted surfaces (see high resolution spectra in [Figure S1](#)).  
173 The quantification of those contributions indicated that the monomer surface density was  
174 much lower in the case of the thermal grafting than for the UV and Mohr's salt catalyzed  
175 grafting ([Figure 1A](#)).

176 Specifically, the S/C ratio for the UV and Mohr's salt samples was more than ten times higher  
177 than for thermal grafting ([Figure 1A](#)). The PNaSS surface density (SD) by UV irradiation was  
178 higher than when using Mohr's salt. The ranking was  $SD_{\text{UVG-PET}} > SD_{\text{MSG-PET}} > SD_{\text{TG-PET}}$ . Whilst  
179 the XPS confirms the presence of PNaSS, the % S/C values themselves are small indicating that  
180 the layers are thin and most probably patchy. Indeed, a rough estimate value for the UVG  
181 PNaSS average layer thickness of  $0.05$  nm can be deduced from a simple homogeneous model  
182 based on the depth probed by XPS being equal to  $10$  nm ([Figure S2](#)) and calculations  
183 thereafter.

184 Nevertheless, the surfaces were more hydrophilic after functionalization (Figure S3) and the  
185 surface energy showed some correlation with the XPS results. The surface tension ( $\gamma_s$ ) of  
186 functionalized surfaces was measured by the contact angle method (Figure 1B). Non-grafted  
187 and TG-PETs were similar:  $\sim 45$ - $48$  mN/m. However, surface tension increased significantly  
188 on UV grafting samples. Particularly,  $\gamma_s$  of UVG-PET increased by 54 % (73 mN/m) and 8 % for  
189 MSG-PET ( $\sim 52$  mN/m). These variations correlate with the amount of  $\text{SO}_3^-$  groups (% Sulfur  
190 by XPS) on the surface leading to the increase of surface tension (represented by the S/C ratio  
191 in Figure 1A).



192  
193 Figure 1. Surface characterization of non-grafted-ozonized and grafted PET: (a) S/C ratio from  
194 XPS and (b) surface tension by contact angle

195

### 196 3.2. Investigating structure of PNaSS-grafted PET surface by AFM

197 The surface SEM images showed no obvious changes (Figure S4). Therefore, in this work, we  
198 investigated the grafted surface using atomic force microscope (AFM). AFM can be used as a  
199 non-destructive method to analyze polymer surfaces[28,30–33]. Numerous parameters can  
200 be investigated, e.g. the macromolecule structure[18], thickness[34–39], and adhesion.  
201 PNaSS-grafted PET surfaces were investigated by AFM peak force Quantitative Nano-  
202 mechanical properties (PF-QNM) in air at room temperature and compared to non-grafted-  
203 ozonized surface. Adhesion maps measure the interaction between the AFM tip and the  
204 material : they can therefore provide clues as to the local chemical nature of the surface[40].

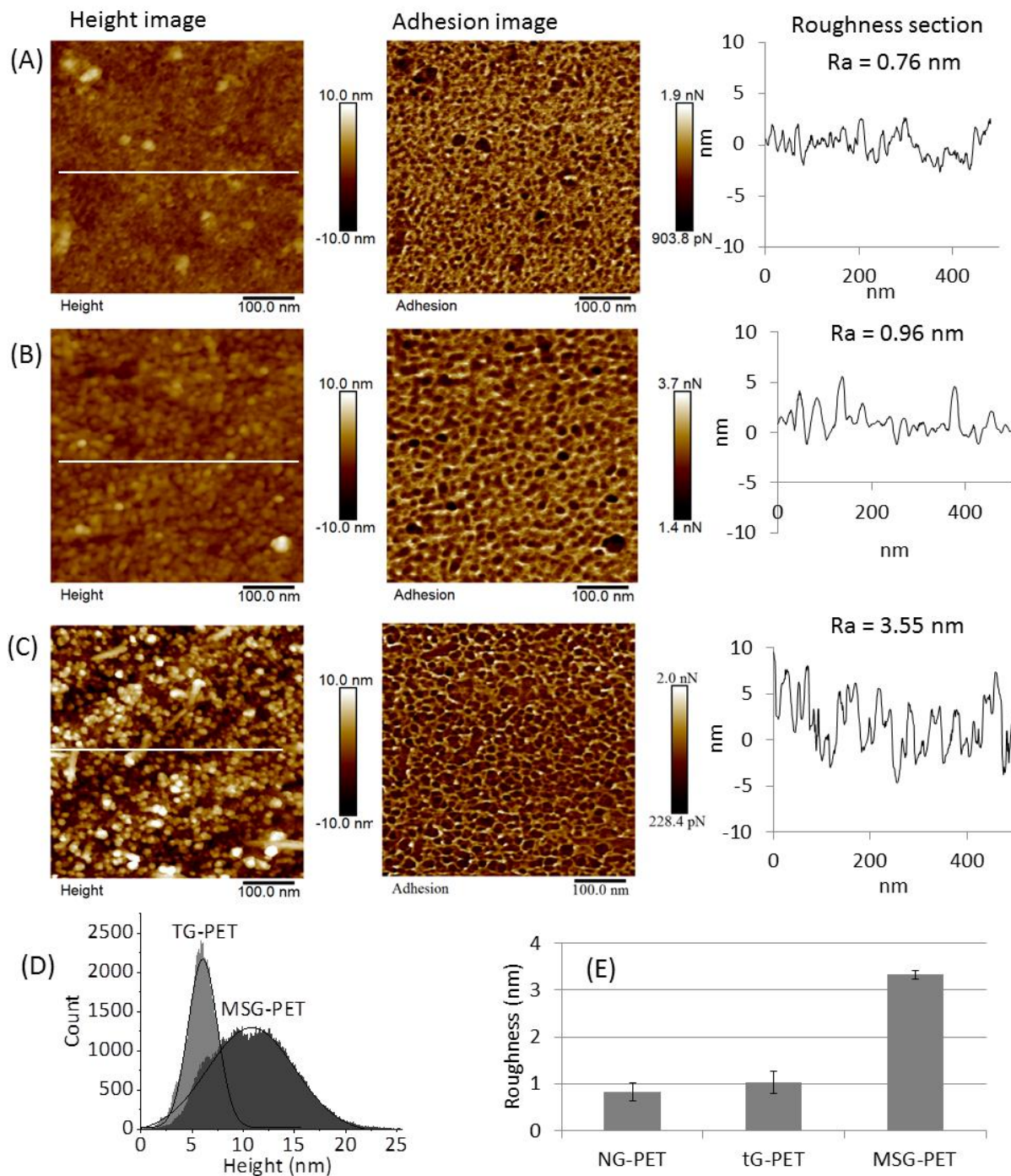


205 The surface topography and adhesion images of non-grafted-ozonized PET were used as a  
206 reference. The AFM images of the PET surfaces obtained after PNaSS grafting by the thermal  
207 grafting and Mohr's salt grafting methods are shown in [Figure 2](#) and briefly described below.

#### 208 **Thermal radical polymerization:**

209 **Thermal grafting.** TG-PET surface topography and adhesion were similar to the non-grafted-  
210 ozonized surface ([Figure 2A-B](#)). This was in agreement with the XPS and contact angle results  
211 which suggested a low degree of grafting. The surface roughness of TG-PET ( $R_a = 0.76$  nm)  
212 was similar with that of non-grafted PET ( $R_a = 0.96$  nm), see in [Figure 2E](#).

213 **Thermal grafting in the presence of Mohr's salt.** The topography of MSG-PET appeared  
214 similar but the surface roughness ( $R_a = 3.55$  nm, see in [Figure 2C](#)) increased by a factor 3  
215 ([Figure 2E](#)).



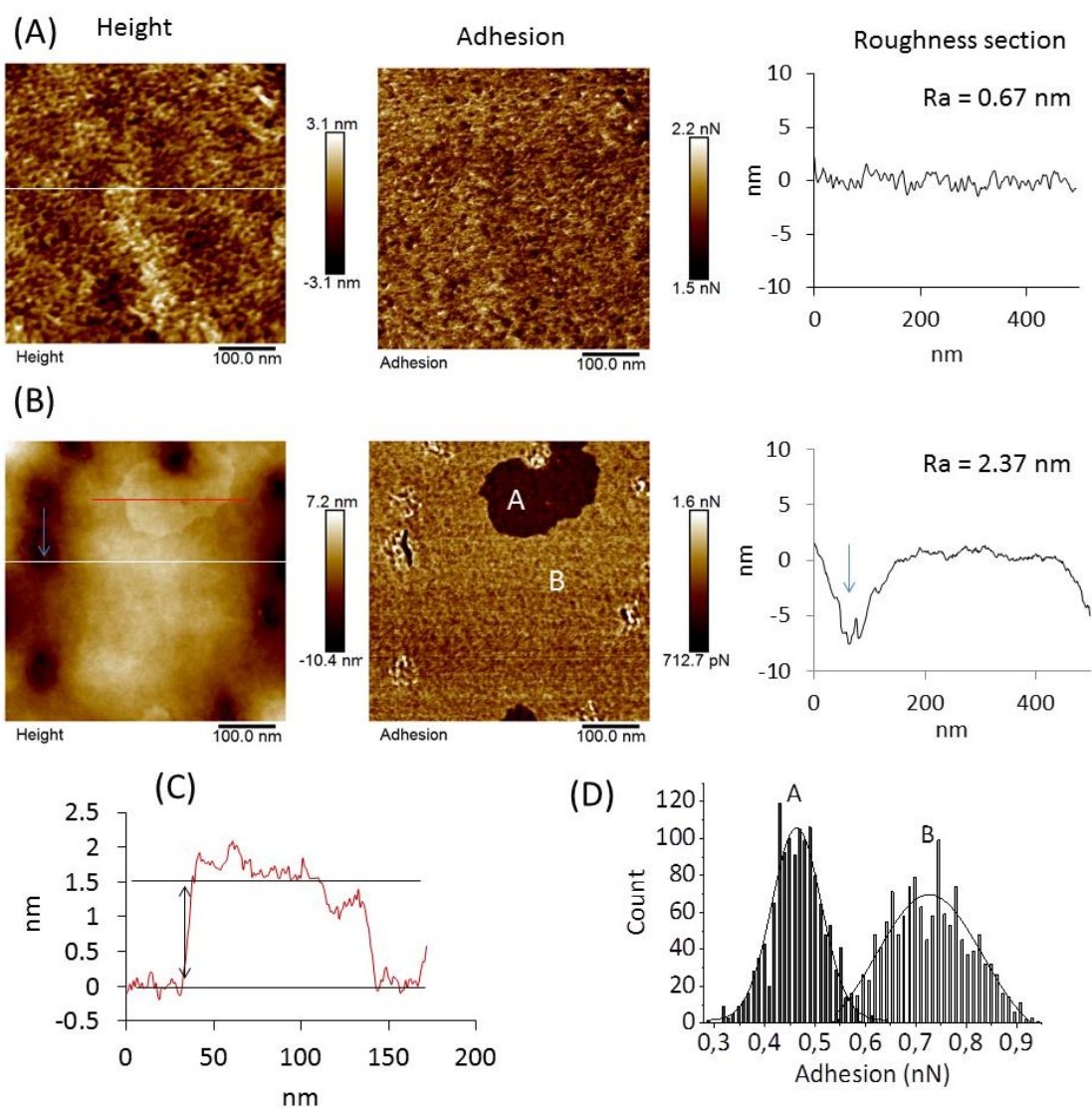
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217 Figure 2. AFM images of non-grafted and thermal grafted PET: (A) non-grafted-ozonized PET  
 218 without grafting, (B) thermal grafting (TG-PET), (C) thermal grafting in the presence of Mohr's  
 219 salt (MSG-PET), (D) Height distribution of TG-PET and MSG-PET, (E) Roughness values for each  
 220 method; Scan in air, scan size 500 nm x 500 nm, 256 points/line, scan rate 1 Hz, PF-QNM

221

222 **Photoinitiated radical polymerization:**

223 **UV grafting (UVG).** Remarkably, in the case of UV grafting, both topography and adhesion  
224 images (Figure 3) were drastically different from what had been observed in the other cases.  
225 To evaluate whether the UV treatment itself had an effect on surface topography, a control  
226 sample was prepared with non-grafted-ozonized PET under UV irradiation for 30 min without  
227 monomer. No major difference between this UV control (Figure 3A) and the non-grafted-  
228 ozonized control (Figure 2A) were observed. To the contrary, a smoother surface was  
229 observed on UV grafted PET with patches particularly striking in the adhesion image (Figure  
230 3B). The patch shown in Figure 3C is  $\sim 1.5$  nm thick (red line) and with reduced adhesion  
231 (Figure 3D). An average thickness of the patches can be deduced from multiple measurements  
232 of different patches ( $\sim 1.2$  nm,  $n = 5$ , Figure S5). Taking into account the surface covered by  
233 the patches ( $\sim 8\%$  of the total area, Figure S5) the thickness averaged overall the whole area  
234 is  $\sim 0.09$  nm ( $8\% \times 1.2$  nm), consistent with the XPS results ( $\sim 0.05$  nm, see above and Figure  
235 S2) suggesting that those patches are indeed composed of PNaSS.



236

237 Figure 3. AFM images of UV grafted PET (A) Control sample (ozonized PET under UV irradiation  
 238 without monomer), (B) UV grafted PET, (C) Particular Cross-section by red line, and (D)  
 239 Adhesion force distribution (flat surface, patches); scan size 500 nm x 500 nm, 256 points/line,  
 240 scan rate 1 Hz, PF-QNM

241

#### 242 4. Discussion

243 The combination of the XPS, surface tension and AFM images suggest the following picture of  
 244 the grafted surfaces. The thermal grafting results indicate a low grafting (XPS results, [Figure](#)  
 245 [1A](#)) on PET. This correlates with the surface tension measurements where we do not observe  
 246 significant changes from the unmodified surfaces ([Figure 1B](#)). The AFM images of those  
 247 surfaces in dry air may not allow visualization of the PNaSS in the case of thermal grafting.

248 The absence of detectable change in the case of thermal grafting is probably due to a  
249 combination of low grafting (as indicated by XPS and surface tension) and of the fact that the  
250 non-grafted-ozonized PET surface is already rough making it harder to detect small changes.  
251 In the case of thermal grafting in the presence of Mohr's salt, XPS and surface tension  
252 measurements correlate and both point to an increased functionalization. The AFM images  
253 show an increased roughness (Figure 2 and Figure S6) but this increase cannot be attributed  
254 to PNaSS because we know from the XPS results that on average the PNaSS layer is only of  
255 the order of  $\sim 0.02$  nm suggesting a low coverage of thin patches (Figure S2). Instead, the  
256 increase of the surface roughness is probably caused by surface degradation in the presence  
257 of Mohr's salt redox initiator as previously reported [40].  
258 In the case of photoinitiated radical polymerization (UV grafting), again XPS and surface  
259 tension measurements correlate (Figure 1). Compared to Mohr's salt, they point to an  
260 increased PNaSS surface density for PET. In the AFM images we observe  $\sim 1$  nm thick patches  
261 covering 8% of the surface and with markedly reduced adhesion. We interpret those patches  
262 as being PNaSS patches since they correspond to the average thickness estimated by XPS. We  
263 note that the rest of the surface show a different (smoother) structure compared to the  
264 control. We used an ozonized PET under UV irradiation in distilled water to evaluate if changes  
265 to surface topology could have been caused by the UV irradiation treatment but that does  
266 not seem to be the case. Further investigations will be needed to determine what causes the  
267 smoothening of the PET surface during PNaSS grafting by UV irradiation. Another limitation  
268 of our interpretation of the results is that those unexplained topography changes could have  
269 contributed to the variations of contact angle independently of PNaSS coverage.

270

## 271 **5. Conclusion**

272 PNaSS was successfully immobilized by ozonation activation and thermal grafting or UV  
273 grafting. The results provide insights into the morphology of PNaSS grafted on polyethylene  
274 terephthalate that is commonly used in biomedical engineering by harnessing a combination  
275 of AFM-Peakforce Quantitative Nanomechanical properties with XPS and contact angle  
276 measurements. Average thicknesses in the nm or sub-nm range determined by XPS indicate  
277 a low PNaSS coverage. In the case of UV grafting 1 nm thick discrete patches covering  $\sim 8\%$  of  
278 the surface were observed. Some surface reconstruction happening during PNaSS grafting will

279 need to be explored in further work. As said in the introduction, the reported findings would  
280 allow precisng how the pNaSS molecules can interact with specific proteins as fibronectin  
281 and by this with cells. A lot of in vitro and in vivo biological results were obtained and  
282 published on pNaSS grafted PET and this precise and fine view in the structure of the grafted  
283 molecules will be a perfect tool to perfect the elucidation of the mechanism of the biological  
284 activity of such surfaces.

285

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289

## 290 **References**

- 291 [1] Felgueiras H P, Sommerfeld S D, Murthy N S, Kohn J and Migonney V 2014 Poly(NaSS)  
292 functionalization modulates the conformation of fibronectin and collagen type i to  
293 enhance osteoblastic cell attachment onto Ti6Al4V *Langmuir* **30** 9477–83
- 294 [2] Vaquette C, Viateau V, Guérard S, Anagnostou F, Manassero M, Castner D G and  
295 Migonney V 2013 The effect of polystyrene sodium sulfonate grafting on  
296 polyethylene terephthalate artificial ligaments on invitro mineralisation and invivo  
297 bone tissue integration *Biomaterials* **34** 7048–63
- 298 [3] Curti P S, Moura M R D, Veiga W, Radovanovic E, Rubira A F and Muniz E C 2005  
299 Characterization of PNIPAAm photografted on PET and PS surfaces *Appl. Surf. Sci.* **245**  
300 223–33
- 301 [4] Elbert D L, Herbert C B and Hubbell J A 1999 Thin polymer layers formed by  
302 polyelectrolyte multilayer techniques on biological surfaces *Langmuir* **15** 5355–62
- 303 [5] Girard J, Brunetto P S, Braissant O, Rajacic Z, Khanna N, Landmann R, Daniels A U and  
304 Fromm K M 2013 Development of a polystyrene sulfonate/silver nanocomposite with  
305 self-healing properties for biomaterial applications *Comptes Rendus Chim.* **16** 550–6
- 306 [6] Simoes J A, Citron D M, Aroutcheva A, Anderson R A, Chany C J, Waller D P, Faro S

- 307 and Zaneveld L J D 2002 Two novel vaginal microbicides (polystyrene sulfonate and  
308 cellulose sulfate) inhibit Gardnerella vaginalis and anaerobes commonly associated  
309 with bacterial vaginosis *Antimicrob. Agents Chemother.* **46** 2692–5
- 310 [7] Chouirfa H, Evans M D M, Bean P, Saleh-Mghir A, Crémieux A C, Castner D G,  
311 Falentin-Daudré C and Migonney V 2018 Grafting of Bioactive Polymers with Various  
312 Architectures: A Versatile Tool for Preparing Antibacterial Infection and  
313 Biocompatible Surfaces *ACS Appl. Mater. Interfaces* **10** 1480–91
- 314 [8] Chouirfa H, Evans M D M, Castner D G, Bean P, Mercier D, Galtayries A, Falentin-  
315 Daudré C and Migonney V 2017 Grafting of architecture controlled poly(styrene  
316 sodium sulfonate) onto titanium surfaces using bio-adhesive molecules: Surface  
317 characterization and biological properties *Biointerphases* **12** 02C418
- 318 [9] Harris C M, Miller S G, Andresen K and Thompson L B 2018 Quantitative  
319 measurement of sodium polystyrene sulfonate adsorption onto CTAB capped gold  
320 nanoparticles reveals hard and soft coronas *J. Colloid Interface Sci.* **510** 39–44
- 321 [10] Su N, Li H B, Zheng H M, Yi S P and Liu X H 2012 Synthesis and characterization of  
322 poly(sodium-p-styrenesulfonate)/modified SiO<sub>2</sub> spherical brushes *Express Polym.*  
323 *Lett.* **6** 680–6
- 324 [11] Moujahid E M, Besse J P and Leroux F 2002 Synthesis and characterization of a  
325 polystyrene sulfonate layered double hydroxide nanocomposite. In-situ  
326 polymerization vs. polymer incorporation *J. Mater. Chem.* **12** 3324–30
- 327 [12] Börner H G, Duran D, Matyjaszewski K, Da Silva M and Sheiko S S 2002 Synthesis of  
328 molecular brushes with gradient in grafting density by atom transfer polymerization  
329 *Macromolecules* **35** 3387–94
- 330 [13] Rohman G, Huot S, Vilas-Boas M, Radu-Bostan G, Castner D G and Migonney V 2015  
331 The grafting of a thin layer of poly(sodium styrene sulfonate) onto poly( $\epsilon$ -  
332 caprolactone) surface can enhance fibroblast behavior *J. Mater. Sci. Mater. Med.* **26**  
333 206
- 334 [14] Nguyen T N, Rangel A A, Migonney V, Nguyen N T, Rangel A A and Migonney V 2020  
335 Kinetic and degradation reactions of poly (sodium 4-styrene sulfonate) grafting



- 336 “from” ozonized poly ( $\epsilon$ -caprolactone) surfaces *Polym. Degrad. Stab.* **176** 109154
- 337 [15] Lego B, Skene W G and Giasson J S 2008 Unprecedented covalently attached ATRP  
338 initiator onto OH-functionalized mica surfaces *Langmuir* **24** 379–82
- 339 [16] Mathis C H, Simič R, Kang C, Ramakrishna S N, Isa L and Spencer N D 2019 Indenting  
340 polymer brushes of varying grafting density in a viscous fluid: A gradient approach to  
341 understanding fluid confinement *Polymer (Guildf)*. **169** 115–23
- 342 [17] Ciobanu M, Siove A, Gueguen V, Gamble L J, Castner D G and Migonney V 2006  
343 Radical graft polymerization of styrene sulfonate on poly(ethylene terephthalate) films  
344 for ACL applications: “Grafting from” and chemical characterization  
345 *Biomacromolecules* **7** 755–60
- 346 [18] Yamamoto S, Ejaz M, Tsujii Y and Fukuda T 2000 Surface interaction forces of well-  
347 defined, high-density polymer brushes studied by atomic force microscopy. 2. Effect  
348 of graft density *Macromolecules* **33** 5608–12
- 349 [19] Yamamoto S, Tsujii Y and Fukuda T 2000 Atomic force microscopic study of stretching  
350 a single polymer chain in a polymer brush *Macromolecules* **33** 5995–8
- 351 [20] Jones D M, Brown A A, Huck W T S, Street P and Cb C 2002 Surface-Initiated  
352 Polymerizations in Aqueous Media: Effect of Initiator Density Darren *Langmuir* 1265–  
353 9
- 354 [21] Fujimoto K, Takebayashi Y, Inoue H and Ikada Y 1993 Ozone-induced graft  
355 polymerization onto polymer surface *J. Polym. Sci. Part A Polym. Chem.* **31** 1035–43
- 356 [22] Amokrane G, Falentin-Daudré C, Ramtani S and Migonney V 2018 A Simple Method  
357 to Functionalize PCL Surface by Grafting Bioactive Polymers Using UV Irradiation *Irbm*  
358 **39** 268–78
- 359 [23] Ishigaki I, Sugo T, Takayama T, Okada T, Okamoto J and Machi S 1982 Graft  
360 polymerization of acrylic acid onto polyethylene film by preirradiation method. II.  
361 Effects of oxygen at irradiation, storage time after irradiation, mohr’s salt, and  
362 ethylene dichloride *J. Appl. Polym. Sci.* **27** 1043–51
- 363 [24] Fujimoto K, Tadokoro H, Ueda Y and Ikada Y 1993 Polyurethane surface modification



- 364 by graft polymerization of acrylamide for reduced protein adsorption and platelet  
365 adhesion *Biomaterials* **14** 442–8
- 366 [25] Pavon-Djavid G, Gamble L J, Ciobanu M, Gueguen V, Castner D G and Migonney V  
367 2007 Bioactive poly(ethylene terephthalate) fibers and fabrics: Grafting, chemical  
368 characterization, and biological assessment *Biomacromolecules* **8** 3317–25
- 369 [26] Frederick M. Fowkes and Fowkes F M 1964 Attractive Forces At Interfaces *Ind. Eng.*  
370 *Chem.* **56** 40–52
- 371 [27] Hermanowicz P, Sarna M, Burda K and Gabryś H 2014 AtomicJ: An open source  
372 software for analysis of force curves *Rev. Sci. Instrum.* **85**
- 373 [28] Pittenger B, Erina N, Su C, Mapping M P, Pittenger B, Erina N and Su C 2010  
374 Quantitative Mechanical Property Mapping at the Nanoscale with PeakForce QNM  
375 *Bruker Appl. Note AN128 AN128* **12**
- 376 [29] Goh S H, Lee S Y, Zhou X and Tan K L 1999 X-ray Photoelectron Spectroscopic Studies  
377 of Interactions between Styrenic Polymers and Poly(2,6-dimethyl-1,4-phenylene  
378 oxide) *Macromolecules* **32** 942–4
- 379 [30] Nair S S, Wang C and Wynne K J 2019 AFM Peakforce QNM mode for measurement  
380 of nanosurface mechanical properties of Pt-cured silicones *Prog. Org. Coatings* **126**  
381 119–28
- 382 [31] Young T J, Monclus M A, Burnett T L, Broughton W R, Ogin S L and Smith P A 2011  
383 The use of the PeakForce™ quantitative nanomechanical mapping AFM-based  
384 method for high-resolution Young's modulus measurement of polymers *Meas. Sci.*  
385 *Technol.* **22**
- 386 [32] Dokukin M E and Sokolov I 2012 Quantitative mapping of the elastic modulus of soft  
387 materials with HarmoniX and PeakForce QNM AFM modes *Langmuir* **28** 16060–71
- 388 [33] Kaemmar S B 2011 Introduction to Bruker's ScanAsyst and PeakForce Tapping AFM  
389 Technology *Appl. note* **133** 12
- 390 [34] Sui X, Zapotoczny S, Benetti E M, Schön P and Vancso G J 2010 Characterization and  
391 molecular engineering of surface-grafted polymer brushes across the length scales by

- 392 atomic force microscopy *J. Mater. Chem.* **20** 4981–93
- 393 [35] Chen W L, Cordero R, Tran H and Ober C K 2017 50th Anniversary Perspective:  
394 Polymer Brushes: Novel Surfaces for Future Materials *Macromolecules* **50** 4089–113
- 395 [36] Halperin A and Zhulina E B 2010 Atomic force microscopy of polymer brushes:  
396 Colloidal versus sharp tips *Langmuir* **26** 8933–40
- 397 [37] Phillips R W 1994 Atomic force microscopy for thin film analysis *Surf. Coatings*  
398 *Technol.* **68–69** 770–5
- 399 [38] Lego B, Skene W G and Giasson S 2010 Swelling study of responsive polyelectrolyte  
400 brushes grafted from mica substrates: Effect of pH, salt, and grafting density  
401 *Macromolecules* **43** 4384–93
- 402 [39] Variola F 2015 Atomic force microscopy in biomaterials surface science *Phys. Chem.*  
403 *Chem. Phys.* **17** 2950–9
- 404 [40] Zalakain I, Politakos N, Ramos J A, Saralegi A, Etxeberria H, Mondragon I, Corcuera M  
405 A and Eceiza A 2013 Chemical and morphological characterization of sulfonated  
406 polystyrene brushes in different environments *Eur. Polym. J.* **49** 2120–7

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#### 408 **Declaration of interests**

409 The authors declare that they have no known competing financial interests or personal  
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#### 412 **Author Contributions**

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415 [Interpretation of data, draft and substantively revised the work.](#) **Vincent Humblot:**  
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