Duo-bimorph actuator made of PMN-PT [011]: 3D modeling, development and characterization

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Abstract— This paper reports the development of a duo-bimorph cantilevered actuator made of PMN-PT material and intended for large-stroke micro-scale manipulation. The principle of operation is piezoelectric, but with a series of material-induced particularities: PMN-PT is reputed for its very high piezoelectric and electromechanical coupling characteristics, but exhibits a lower coercive field which prevents driving in a fully bipolar manner. Instead of the uniaxial [001] plate, by using the anisotropic [011] cut, a positive transverse $d_{31}$ piezoelectric coefficient may be exploited. This allows the extension of the structure with the applied voltage, which is particularly beneficial for micro-gripping. After an introductory part in piezo-materials and duo-bimorph structures, a comprehensive static three-dimensional displacement modeling is provided by means of constitutive matrix equations. The actuator micro-manufacturing is presented, followed by the experimental characterization. Compared to the classical PZT structures, the actuation is increased by a factor of two, up to 600 µm in the transversal plane and up to 20 µm longitudinally. Some perspectives related to 3 DoF (Degrees of Freedom) micro-manipulation tasks are finally approached.

I. INTRODUCTION

Nowadays, the microsystems functional requirements keep ever increasing. Many products notably require the integration of smart materials for actuation and/or sensing purposes. Applications such as in the Micro-Electro-Mechanical-Systems (MEMS) [1], biomedical [2][3], microrobotics or microgripping [4] must take advantage of highly integrated, very accurate and highly dynamic smart materials.

Among the smart materials, piezoelectric ones are widespread because they enable generating accurate, multi DoF motions with large bandwidth and forces. Despite these advantages, new piezo materials are being developed to obtain increased performance. For example, studies in the microrobotic and micro-assembly fields have shown that DoF must be placed closer to the manipulated object, i.e. dexterous microgripper are desirable with respect to the basic grippers moved by robotic structures [5][6]. Many piezoelectric microgripppens have been proposed, some of them proposing 4 DoF [7] (both fingers actuated up and down supplementary to the open and close motions), thus offering increased gripping dexterity. Innovative materials or manufacturing techniques (PMN-PT, sol-gel etc.) present several advantages over the commonly-used sintered piezo-ceramics (PZT), especially in terms of displacement range or integration. This paper will focus on the use of PMN-PT materials because they are capable of much larger actuation [8] and more degrees of freedom for similar free space (extremely high ferroelectric properties for all directions).

PMN-PT materials are quite recent (available since the 2000’s) and their behavior is still to be fully investigated in applications. PMN-PT actuators can be manufactured using microfabrication techniques [9] and can thus be structured easier than other kinds of piezo-materials [10]. This paper will continue the aim at studying the PMN-PT material properties and particularities, this time investigating the particularly interesting anisotropic cut in the [011] poling direction. The difference to the regular and uniaxial [001] cut, is that the [011] PMN-PT exhibit a positive transverse piezoelectric coefficient in the X direction and an even larger, negative coefficient in the Y crystalline direction. This particularity allows the extension of the beam structure with the applied voltage rather than compression, which is particularly beneficial for micro-gripping.

This paper case of study is a duo-bimorph cantilever beam, which is an interesting multi DoF test-bed to compare the PMN-PT materials with more classical ones like PZT. Provided the advantage of positive transverse piezoelectric coefficient in [011] and the extension of the structure to the applied voltage, the third longitudinal axis could be exploited in a micro-gripper configuration.

The paper is structured as follows: Section II will present the 3D displacement modeling aspects in an analytical constitutive form. Section III will display the experimental results inducing model validation and coupling issues. A conclusion highlighting the specificities and advantages of PMN-PT will end the paper.

II. DUO-BIMORPH MODELING

A. Presentation of the duo-bimorph structure

A duo-bimorph actuator is made up of two layers of piezoelectric material soldered or bonded together, like a regular bimorph actuator. The difference consists of having five electrodes instead of three, like in Figure 1. Thus, by using a proper combination of signals, displacement in Y direction becomes possible.

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Figure 1. Structure of the duo-bimorph actuator, the electrode convention and the working referential system.

Depending on the two layers poling direction and on the piezoelectric transverse coefficients signs, a strict convention must be established for the applied voltages as shown in Figure 2.

\[\begin{align*}
\delta_x^+: &+V_{E1}+V_{E2}+V_{E3}+V_{E4} \\
\delta_x^-: &+V_{E1}+V_{E2}-V_{E3}-V_{E4} \\
\delta_y^+: &+V_{E1}+V_{E2}-V_{E3}+V_{E4} \\
\delta_y^-: &+V_{E1}-V_{E2}-V_{E3}+V_{E4} \\
\delta_z^+: &+V_{E1}+V_{E2}+V_{E3}-V_{E4} \\
\delta_z^-: &+V_{E1}+V_{E2}-V_{E3}-V_{E4}
\end{align*}\]

Figure 2.a) Same direction poling duo-bimorph (side view); b) opposite-direction poling duo-bimorph. The difference consist in the applied voltages signs to obtain the desired displacement.

**B. Modeling of the duo-bimorph**

The first modeling of a duo-bimorph piezo-beam has been performed in [11]. Provided the PMN-PT particularities, the constitutive equations should be updated for PMN-PT because of the lower (limited) coercive field [8]. Still provided the large actuation, adding the modeling of the duo-bimorph in the third longitudinal X-direction is also preferable. Finally, the end-effector modeling will be added.

As already noticed in Figure 1, the duo-bimorph displacement is controlled by applying high voltage signals to the 4 electrodes \((V_{E1}, V_{E2}, V_{E3}, \text{ and } V_{E4})\). The complete 3D voltage-to-displacement model may be expressed as follows:

\[\left\{\begin{array}{l}
\delta_x \\
\delta_y \\
\delta_z
\end{array}\right\} = (C + F) \cdot S \cdot V_E \]  

(1)

Where \(\delta_x, \delta_y, \delta_z\) are the deflections on the X, Y and Z axes, \(V_E\) is the array of voltages across the electrodes, \(C\) is the piezo-bimorph constitutive matrix and \(F\) is the end-effector displacement matrix which is effective only transversally:

\[V_E = \begin{bmatrix}
V_{E1} \\
V_{E2} \\
V_{E3} \\
V_{E4}
\end{bmatrix} \quad C = \begin{bmatrix}
C_{11} & 0 & 0 \\
0 & C_{22} & 0 \\
0 & 0 & C_{33}
\end{bmatrix} \quad F = \begin{bmatrix}
0 & 0 & 0 \\
0 & F_{22} & 0 \\
0 & 0 & F_{33}
\end{bmatrix} \]  

(2)(3)(4)

The coefficients \(C_{11}\) to \(F_{33}\) are calculated starting from the strain-charge constitutive matrix of the piezoelectric effect. Due to space restrictions, only the results are shown:

\[C_{11} = \frac{d_{31} L}{4h_p} \]  

(5)

By using the modeling from [11] we derived:

\[C_{22} = \frac{3d_{31} L^2 (w^2 - w_0^2)}{4Al_{1p} w^3} \]  

(6)

\[C_{33} = \frac{3d_{31} L^2 (w - w_0)(h_p + h_g)}{2B_{1p} w} \]  

(7)

And by remodeling the equation described in [7], to fit the duo-bimorph, we derived:

\[F_{22} = \frac{3d_{31} L^2 (w^2 - w_0^2)}{2A_{11} w^3} \]  

(8)

\[F_{33} = \frac{3d_{31} L^2 (w - w_0)(h_p + h_g)}{B_{11} w} \]  

(9)

Where [11]:

\[A = \frac{2h_p + E_g h_g}{s_{11p}} \]  

(10)

\[B = \frac{2h_p (3h_p^2 + 6h_g h_p + 4h_g^2) + E_g h_g^3}{s_{11p}} \]  

(11)

Table 1 explains and provides values for all the above dimensions, parameters and coefficients. In the case of a beam cut along Y-direction, \(s_{11p}\) and \(d_{31}\) coefficients should be replaced by \(s_{22p}\) and \(d_{32}\).

**TABLE I. THE CONSTITUTIVE EQUATIONS PARAMETERS.**

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Description</th>
<th>Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>(L)</td>
<td>Piezo-beam length</td>
<td>23 mm</td>
</tr>
<tr>
<td>(L_w)</td>
<td>End-effector length</td>
<td>4 mm</td>
</tr>
<tr>
<td>(w)</td>
<td>Total beam width</td>
<td>600 µm</td>
</tr>
<tr>
<td>(w_g)</td>
<td>Groove width (electrodes gap)</td>
<td>100 µm</td>
</tr>
<tr>
<td>(h_p)</td>
<td>Piezo-layer thickness</td>
<td>200 µm</td>
</tr>
<tr>
<td>(h_g)</td>
<td>Adhesive-layer thickness</td>
<td>10 µm</td>
</tr>
<tr>
<td>(d_{31})</td>
<td>Transverse piezo coefficient</td>
<td>456.55 pm/V</td>
</tr>
<tr>
<td>(s_{11p})</td>
<td>Piezo elasticity coefficient</td>
<td>69 x 10^{-12} m^2/N</td>
</tr>
<tr>
<td>(E_g)</td>
<td>Young’s modulus of adhesive</td>
<td>1 x 10^12 N/m^2</td>
</tr>
</tbody>
</table>

\(S\) is the sign matrix depending on: the electrodes notation, piezoelectric material poling direction (Figure 2) and the transverse piezoelectric coefficient \((d_{31}\) or \(d_{32}\)\) sign.

Considering the electrode identification shown in Fig.1, the poling in opposite direction of the two PMN-PT layers (as shown in Fig.2.b) and a positive transverse piezoelectric coefficient, conditions which were in our experimental case, the sign matrix, \(S\) is as follows:

\[S = \begin{bmatrix}
-1 & -1 & 1 & -1 \\
1 & -1 & 1 & -1
\end{bmatrix} \]  

(12)

We shall make the following notation of three voltage signals:
\[
V_g = \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix} = \frac{1}{4} S \begin{pmatrix} V_{E1} \\ V_{E2} \\ V_{E3} \\ V_{E4} \end{pmatrix}
\] (13)

By combining expressions (1) with (13), we get the following linear, theoretically decoupled system:
\[
\begin{pmatrix} \delta_X \\ \delta_Y \\ \delta_Z \end{pmatrix} = \left(4(C+F)\right) \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix} = 4(C+F) V_\delta
\] (14)

This expression (model) can be easily reverted to estimate the required voltage for a given displacement:
\[
\begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix} = \frac{1}{4} (C+F)^{-1} \begin{pmatrix} \delta_X \\ \delta_Y \\ \delta_Z \end{pmatrix}
\] (15)

In our case, provided (13), we get the straightforward reverse relation:
\[
\begin{pmatrix} V_{E1} \\ V_{E2} \\ V_{E3} \\ V_{E4} \end{pmatrix} = S^T \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix} = \begin{pmatrix} -1 & 1 & 1 & 1 \\ -1 & -1 & 1 & 1 \\ -1 & -1 & -1 & 1 \end{pmatrix} \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix}
\] (17)

From (15) and (17) we get:
\[
\begin{pmatrix} V_{E1} \\ V_{E2} \\ V_{E3} \\ V_{E4} \end{pmatrix} = S^T \frac{1}{4} (C+F)^{-1} \begin{pmatrix} \delta_X \\ \delta_Y \\ \delta_Z \end{pmatrix}
\] (18)

In the case of piezoelectric materials, the operating voltage must be greater than the one related to the coercive field value, called \( V_C = -E_C \delta_\mu \).

For a 200 \( \mu \)m plate, we experimentally determined the coercive voltage values. These are as follows:
- in the case of PZT, \( V_C = -150 \)V;
- in the case of PMN-PT [001], \( V_C = -45 \)V;
- in the case of PMN-PT [011], \( V_C = -15 \)V.

As noticed, in the case of PMN-PT the \( |V_C| \) is much lower than in the case of PZT. Therefore, we have to restrict the reverse operating field to a safety zone. We call this type of driving: unipolar operation (Figure 3).

For the unipolar operation mode, the restricted voltages are formulated as follows:
\[
\begin{pmatrix} V_{E1}^* \\ V_{E2}^* \\ V_{E3}^* \\ V_{E4}^* \end{pmatrix} = H^* \begin{pmatrix} V_{E1} \\ V_{E2} \\ V_{E3} \\ V_{E4} \end{pmatrix}
\] (19)

Where:
\[
H^* = \begin{pmatrix} H(V_{E1} + V_C) & 0 & 0 & 0 \\ 0 & H(V_{E2} + V_C) & 0 & 0 \\ 0 & 0 & H(V_{E3} + V_C) & 0 \\ 0 & 0 & 0 & H(V_{E3} + V_C) \end{pmatrix}
\] (20)

and \( H(x) \) is the Heaviside step function defined as:
\[
H(x) = \begin{cases} 1, & x \geq 0 \\ 0, & x < 0 \end{cases}
\] (21)

Equation (17) thus becomes:
\[
\begin{pmatrix} V_{E1}^* \\ V_{E2}^* \\ V_{E3}^* \\ V_{E4}^* \end{pmatrix} = H^* S^T \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix}
\] (22)

The resulting displacement for the unipolar case may be expressed in the following manner:
\[
\begin{pmatrix} \delta_X^* \\ \delta_Y^* \\ \delta_Z^* \end{pmatrix} = (C+F) S \begin{pmatrix} V_{E1}^* \\ V_{E2}^* \\ V_{E3}^* \\ V_{E4}^* \end{pmatrix} = (C+F) H^* S^T \begin{pmatrix} V_X \\ V_Y \\ V_Z \end{pmatrix}
\] (23)

C. Coupling modeling/compensation

In the above model, C is an ideal, diagonal matrix.

In real experiment, besides the typical piezoelectric nonlinearities like hysteresis and creep, coupling effects could be present, in this case, some or all off the C-matrix coefficients will be non-zero:
\[
C = \begin{pmatrix} C_{11} & C_{12} & C_{13} \\ C_{12} & C_{22} & C_{23} \\ C_{13} & C_{23} & C_{33} \end{pmatrix}
\] (24)

Coefficients \( C_{11}, C_{22} \) and \( C_{33} \) could be taken from (5-7) but, provided the measurement uncertainty of piezoelectric and stiffness tensors, these coefficients could be also identified experimentally. The remaining unknown coefficients, called coupling coefficients can be identified empirically.

III. EXPERIMENTS WITH PMN-PT DUO-BIMORPH

A. Manufacturing of the micro-actuator featuring positive \( d_{31} \) coefficient in PMN-PT [011] cut

The micro actuator is fabricated starting from two plates of PMN-PT manufactured by TRS Technologies, each 200
µm thick, bonded using a silver-based EPO-TEK® H22 adhesive, 10-20 µm thick.

Individual beams of 600 µm wide, 27 mm long and 410 µm thick were precisely cut using a saw-dicing machine. Prior to this final cut, superficial grooves were patterned on the opposite faces, as shown in Figure 1. These grooves, separating the electrodes $E_1$ from $E_2$ and $E_3$ from $E_4$, are 100 µm wide and 40 µm deep. The middle electrode is the connected to the common ground (GND).

The duo-bimorph beam was aligned in place on a PCB (printed circuit board and glued to the bottom face (E3-E4). The remaining active actuator length is 23mm. The connection between the PCB and electrodes has been done by wire-bonding.

The end-effectors, or MEMS fingertips, are microfabricated in pairs in a silicon-on-insulator (SOI) wafer shaped by Deep-RIE etching whose details are shown in [12]. The top silicon layer is 10µm thick and the end-effectors allow microgripping objects in the 10 to 100 µm range (Figure 4, detail).

The MEMS fingertips are composed of a thick part (413 µm), to be fixed on the actuators, and a thin part (10 µm) with a suitable shape to manipulate the objects. The central part between the two arms is designed to keep the alignment and the gap of the end-effector tips during the assembly process. This central part is removable by means of breakable links present on each side.

![Figure 4. Experimental setup: actuators fixture on the left and the microscopy camera on the right.](image)

**B. Experimental setup**

An imaging setup (Guppy® camera F-036 with 1-7X video tube and 5X long distance Mitutoyo® objective) was placed in front of the actuators to track the displacement of the tips in Y-Z plane (Figure 5). This camera was calibrated in µm using a reference target. The tip displacement position was calculated using image processing software.

![Figure 5. – Image as seen through the Guppy® camera.](image)

Alternately this setup was also used to measure the X-displacement.

The camera was precisely triggered by a dSPACE® 1103 rapid control prototyping controller. A custom-made, high-voltage amplifier was connected between the controller and the piezoelectric actuator (Figure 6).

![Figure 6. Experimental setup for duo-bimorph action and analysis.](image)

**C. Modeling validation**

In order to ascertain whether the model is accurate, certain coefficients needed to be experimentally determined, such as $d_{31}$ and $d_{32}$. These transverse coefficients were calculated separately on the initial plain rectangular plates of 20x25mm² using the same image processing method.

As known [8], PMN-PT [001] has a positive value for $d_{31}$ and a value for $d_{32}$ which is approximately -1/3$d_{31}$. A batch of six plates were individually tested, $d_{31}$ values ranged from 420 pm/V to 485 pm/V and $d_{32}$ ranged from -1000 pm/V to -1360 pm/V. Table II shows the average values. For comparison, we also measured the $d_{31}$ and $d_{32}$ coefficients of some PMN-PT [001] and PZT-5H plates. Coefficient $s_{11} = 69 \times 10^{-12}$ m/N has been taken from [13].

<table>
<thead>
<tr>
<th>Material type</th>
<th>Transverse piezoelectric coefficients</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>$d_{31}$</td>
</tr>
<tr>
<td>PZT-5H</td>
<td>-274 pm/V</td>
</tr>
<tr>
<td>PMN-PT [001]</td>
<td>-924 pm/V</td>
</tr>
<tr>
<td>PMN-PT [001]</td>
<td>+456 pm/V</td>
</tr>
</tbody>
</table>

The experiment was conducted as follows: voltage was applied in step values of 140V, firstly on each electrode $E_1$ to $E_2$ to obtain the displacements in the four quadrants (Figure 7). Then, combined step voltages in $V_1$ and $V_2$ were applied to observe the creep behavior in the transversal plane (Figures 9,10). Finally, sine waveforms were applied to observe the hysteresis and the coupling in all the three directions, including the longitudinal X-axis (Figures 11,12,13). Notice that, to simplify the conditions, only the fully unipolar driving was applied, meaning two electrodes at a time (as in Figure 3.c,d). Table III groups the most relevant experimental results compared with the associate theoretical modeling. Nonlinearities, such as hysteresis, creep and inter-electrode coupling are also numerically presented.

A fair agreement between the analytical modeling and experimental data can be concluded meaning that the user could rely on the provided 3D displacement static mathematical model in his designs.

The nonlinear behavior in terms of creep and hysteresis is under 9%, a very good figure for the PMN-PT material, comparing it to PZT where such nonlinearities are close to 20%.
The actuator has been tested up to ±140V transversally and up to 300V longitudinally. We may notice from Figure 11 that at 300V (15 kV/cm) saturation is far from being reached. This means that such an actuator is viable for a 3D manipulation.

On the other hand, an unwanted coupling can be noticed, which manifests differently along the three axes. The weakest coupling, almost non-existing, is observed on Y-axis when actuating along Z-axis (Figures 11 and 14). This is because the layers are independently actuated. The coupling in Z-axis, when actuating in Y-direction, is larger due to a series of causes which will be detailed in the next paragraph. The largest concern is upon actuating longitudinally (in X-direction). Due to the fact that the longitudinal extension (0.047 µm/V) is much smaller than the transversal flexure (~2 µm/V), coupling in Z-direction was found to exceed 300%, which will require compensation. For instance, by unbalancing the X-voltage by ±10V, the unwanted Z-displacement coupling will be cancelled.

The noticed experimental coupling is, in effect, a combined consequence of several factors. Firstly, there is an inherent difference between the two layers material constants. From Figure 15 we notice a transverse piezoelectric coefficient difference of over 7%. Secondly, in each layer, as three electrodes share a common piezo-element, the electrical field distribution is not decoupled (Figure 9). And thirdly, the cantilevers are not symmetrically clamped (only the bottom layer is bonded) which also induces a certainly unbalanced flexure.

The coupling effect can be better observed and quantified when applying sine wave signals along the three axes (Figure 11 – X-axis, Figure 12 – Y-axis and Figure 13 – Z-axis).

**Figure 7.** Y-Z displacement resulting from step signals applied to individual electrodes: a) $E_1$ only, b) $E_2$ only, c) $E_3$ only, d) $E_4$ only.

**Figure 8.** Representation (FEM simulation) of electric field lines in on of the piezo-layers. Notice the field distribution asymetry.

**Figure 9.** Step input voltage applied on Y-axis. For convenience, the Z-displacement curve was offset by -100 µm.

**Figure 10.** Step input voltage applied on Z-axis. For convenience, the Y-displacement curve was offset by -100 µm.

**Figure 11.** Displacement hysteresis loop in X-axis and the coupling effect in the Z and in the Y axis.

**Figure 12.** Displacement hysteresis loop in Y-axis and the coupling effect in the Z-axis.
investigated and found to be lower than 9\%. Limitations include the unipolar operation mode, due to the material low coercive field, and a certain unwanted coupling between the axes, due to the duo-bimorph structure.

As perspectives, a 3D-capable microgripper could be designed (we already assembled and pictured a first version of the microgripper, which will be treated in a future paper). The coupling has been quantified and due to the modeling complexity will be treated separately.

V. ACKNOWLEDGEMENTS

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